



Analysis of Medical Images based on Computational Methods of Image Registration

João Manuel R. S. Tavares

tavares@fe.up.pt, www.fe.up.pt/~tavares

2º Ciclo de Estudos em
INFORMÁTICA MÉDICA



Presentation

- Associate Professor at the Faculty of Engineering of the University of Porto (FEUP) / Department of Mechanical Engineering
- Senior Research and Projects Coordinator of the Optics and Experimental Mechanics Lab (LOME) of the Institute of Mechanical Engineering and Industrial Management (INEGI)
- PhD and MSc degrees in Electrical and Computer Engineering from FEUP in 2001 and 1995, respectively
- BSc degree in Mechanical Engineering from FEUP in 1992
- Research Areas: Image Processing and Analysis, Medical Imaging, Biomechanics, Human Posture and Control, Product Development



Outline

1. Introduction

2. Methods

a) Spatial Registration of (2D & 3D) Images

b) Spatio & Temporal Registration (2D image sequences)

3. Applications and Results

a) Plantar Pressure Images (2D static images & 2D image sequences)

b) Medical Images (2D & 3D)

4. Conclusions

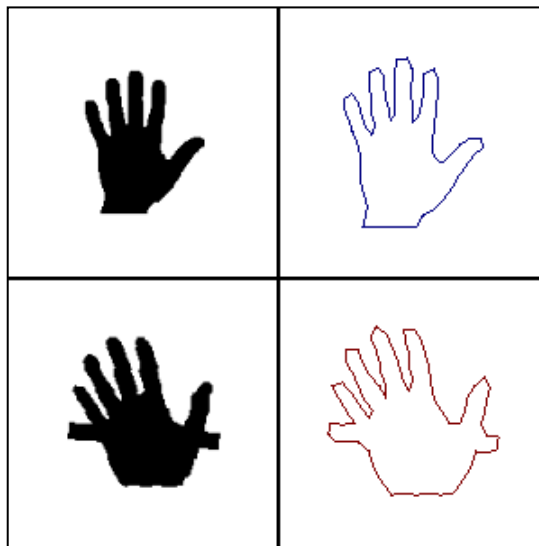


Introduction: Matching and Registration of Images

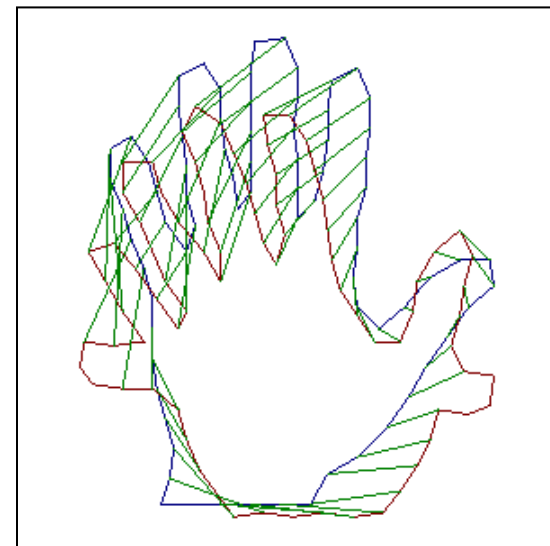


Image Matching

Image matching is **the process of establishing correspondences between objects in images**



Original images and contours



Some of the correspondences found

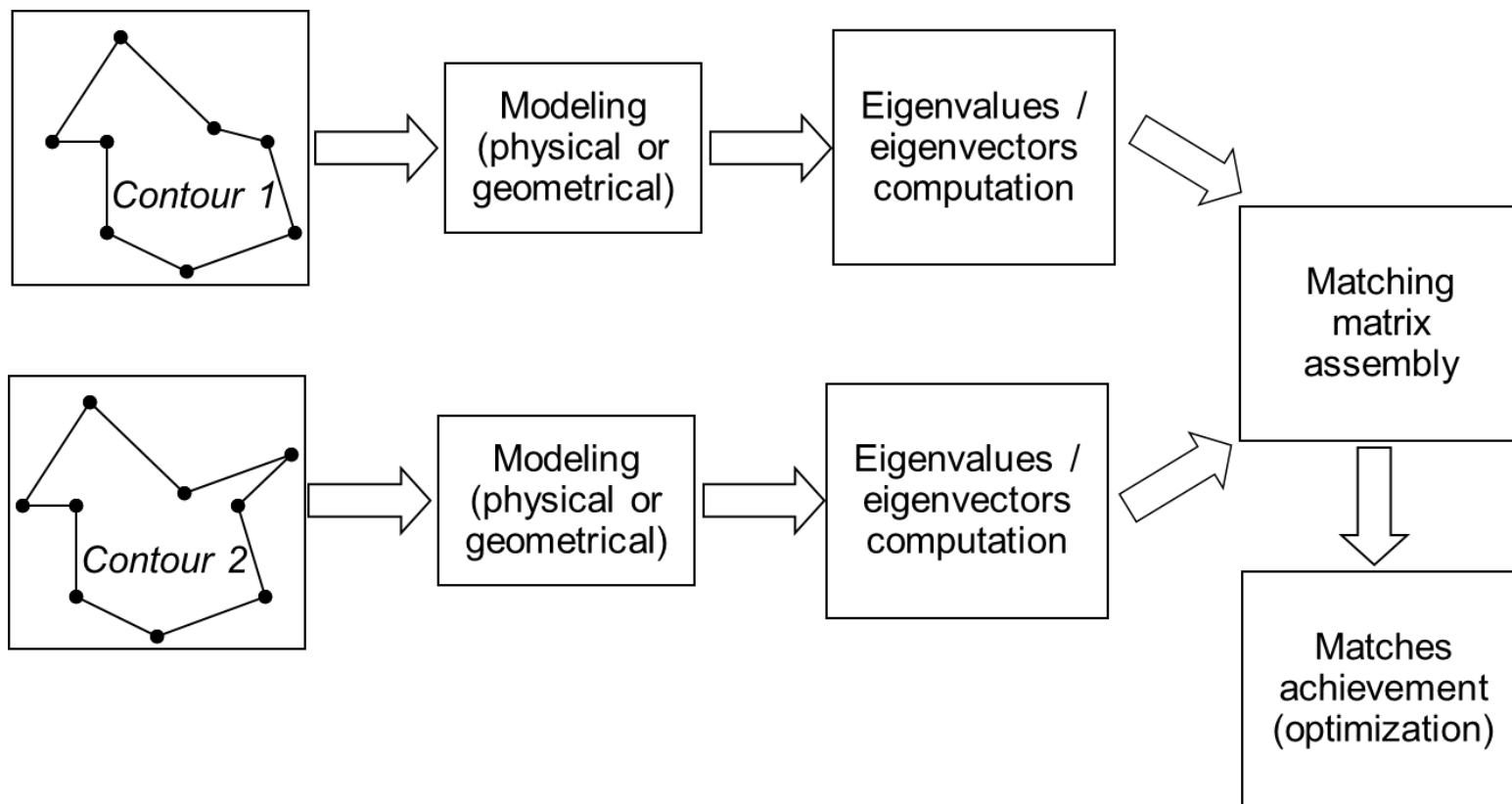
Bastos & Tavares (2006) Inverse Problems in Science and Engineering 14(5):529-541

Oliveira, Tavares, Pataky (2009) VipMAGE 2009, pp. 269-274



Image Matching

Matching based on **physical or geometrical modeling**



Bastos & Tavares (2006) Inverse Problems in Science and Engineering 14(5):529-541

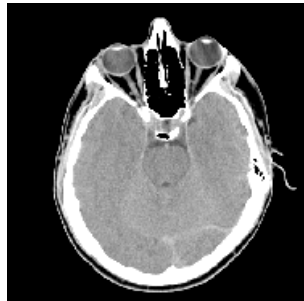
Oliveira, Tavares, Pataky (2009) VipMAGE 2009, pp. 269-274



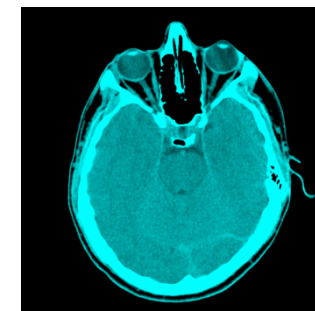
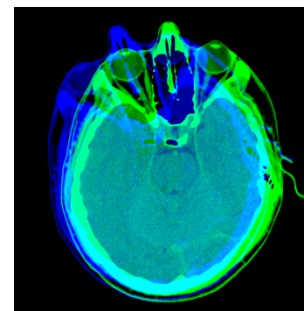
Image Registration

Image registration is the **process of searching for the best transformation that change one image in relation to another image** in order to correlated features assume similar locations in a common space

*Template
(or fixed)
image*



*Source
(or moving)
image*



*Overlapped images before and after
the registration*



Image Registration

The **methodologies can be classified based on** different criteria:

- **Data dimensionality: 2D/2D, 2D/3D, 3D/3D, 2D/3D + Time**
- **Features used: extrinsic** (using features external to the patient) or **intrinsic** (using information from the patient; e.g. pixel or voxel intensity, relevant points, contours, regions, skeletons, surfaces, ...)
- **Interaction: manual, semiautomatic or automatic**
- ...



Image Registration

... cont.

- **Transformation type:** rigid, similarity, affine, projective, curved
- **Transformation domain:** local or global
- **Modalities involved:** same modality (CT/CT, MRI/MRI, PET/PET, ...), different modalities (CT/MRI, MRI-T1/MRI-T2, PET/CT, ...) or **patient/model** (e.g. between a patient and an atlas or between a patient and a device)
- **Subjects:** registration of images from the **same subject** or from **different subjects**, or images of a subject with images in an **atlas**
- **Organs/tissues involved:** brain, liver, etc.
- ...

Oliveira & Tavares (2014) Computer Methods in Biomechanics and Biomedical Engineering 17(2):73-93



Image Registration

Applications

- **Supporting surgical interventions** (more efficient localization of lesions, find alignments between devices and patients, etc.)
- **Optimizing radio-therapeutic treatments**
- **Automatic recognition of organs/tissues** (support complex tasks of image segmentation, analysis and identification, etc.)
- **Building of Atlas** (with well-known cases used for comparison)
- **Simplifying posterior statistical analysis** (SPM, Z-scores, etc.)
- **Simplifying image-based diagnosis**
 - Fusion of images from different imaging modalities (CT/PET, MRI/CT, SPECT/CT, MRI/PET, ...) or points of view
 - Follow-up of pathologies
- ...



Image Registration

In the last years, **we have developed methods for image matching and registration** based on different techniques and applied them in several applications

– Techniques

- Based on **features** (points, contours) extracted from the images and based on the **intensity of the pixels (or voxels)**
- By **computing directly or iteratively the optimal registration transformation**
- By **using different transformation models**

– Data

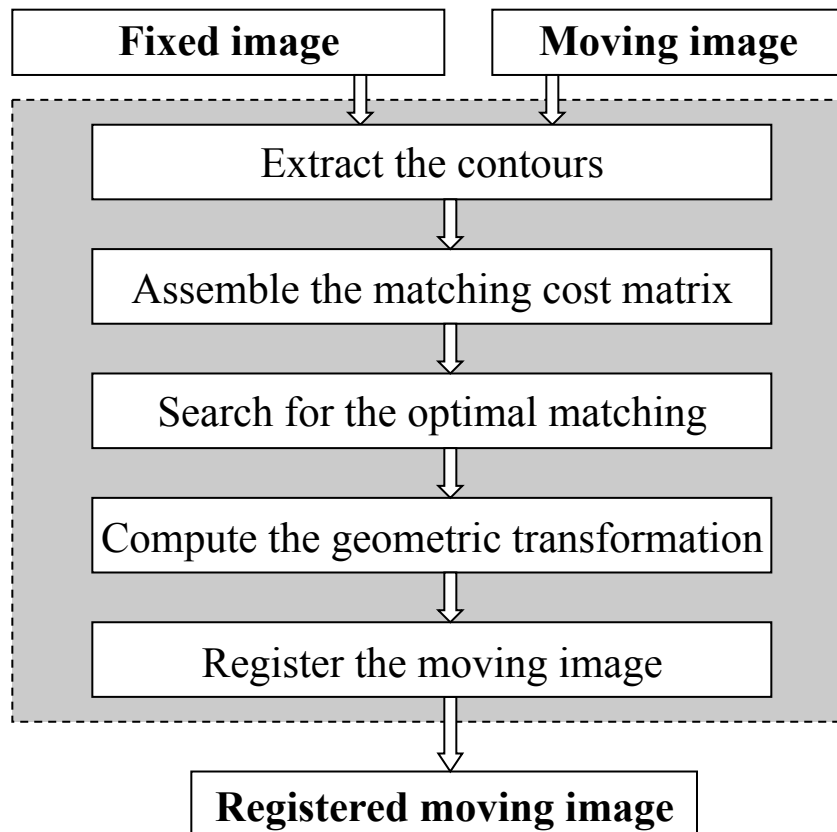
- Images from the **same patient, different patients and atlas**
- Images from the **same or different imaging modalities or different points of view**
- Registration of **2D and 3D images, and of 2D image sequences**



Methods: Spatial Registration of 2D and 3D images



Registration based on Contours Matching



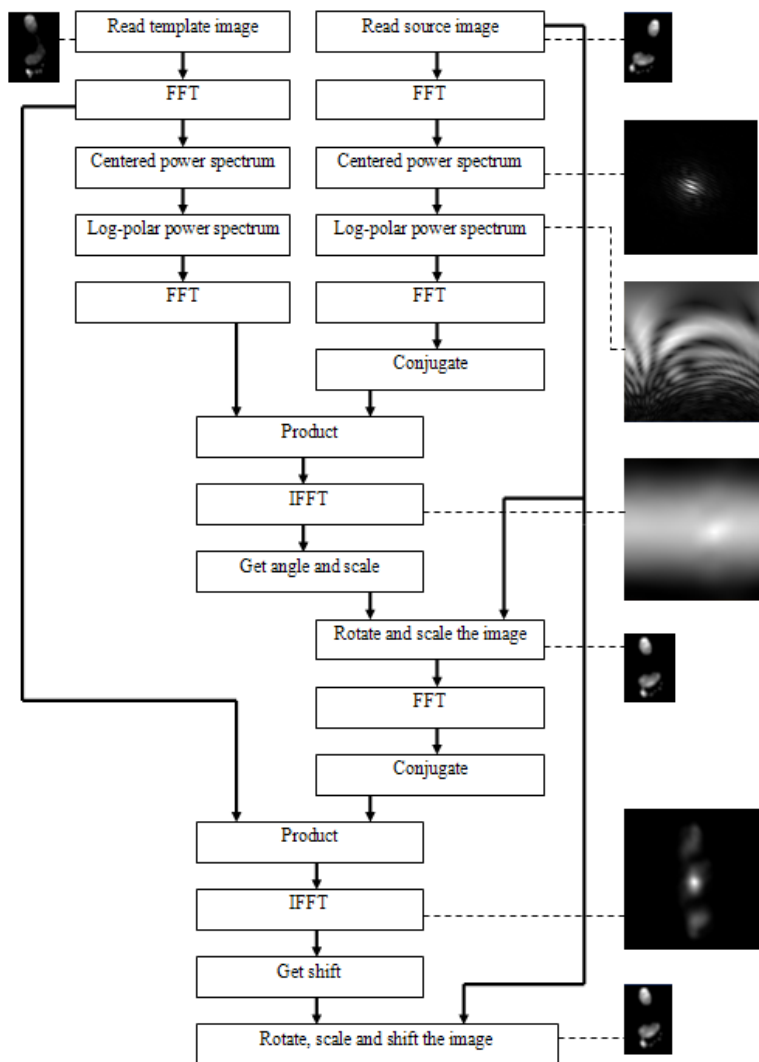
The cost matrix is built based on geometric or physical principles

The matching is found based on the minimization of the sum of the costs associated to the possible correspondences

To search for the best matching is used an optimization assignment algorithm



Registration based on Fourier Transform



The scaling and rotation are obtained from the spectrum images after their conversion to the log-polar coordinate system

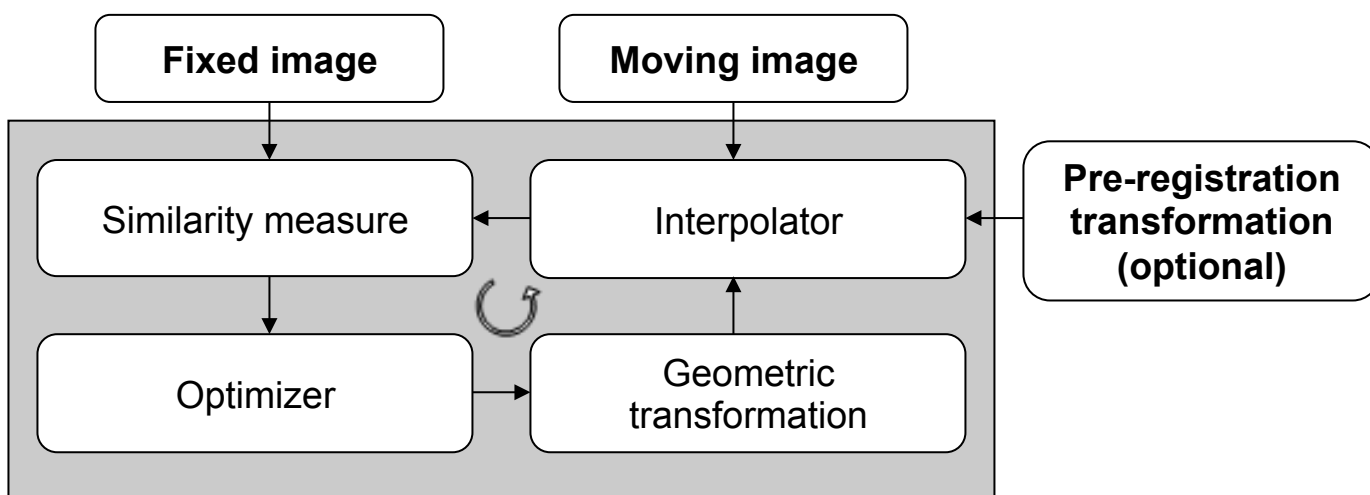
The algorithm searches for the geometric transformation involved using the shift, scaling and rotation properties of the Fourier transform

Oliveira, Pataky, Tavares (2010) *Computer Methods in Biomechanics and Biomedical Engineering* 13(6):731-740



Registration based on Iterative Optimization

Based on the iterative search for the parameters of the transformation that optimizes a similarity measure between the input images

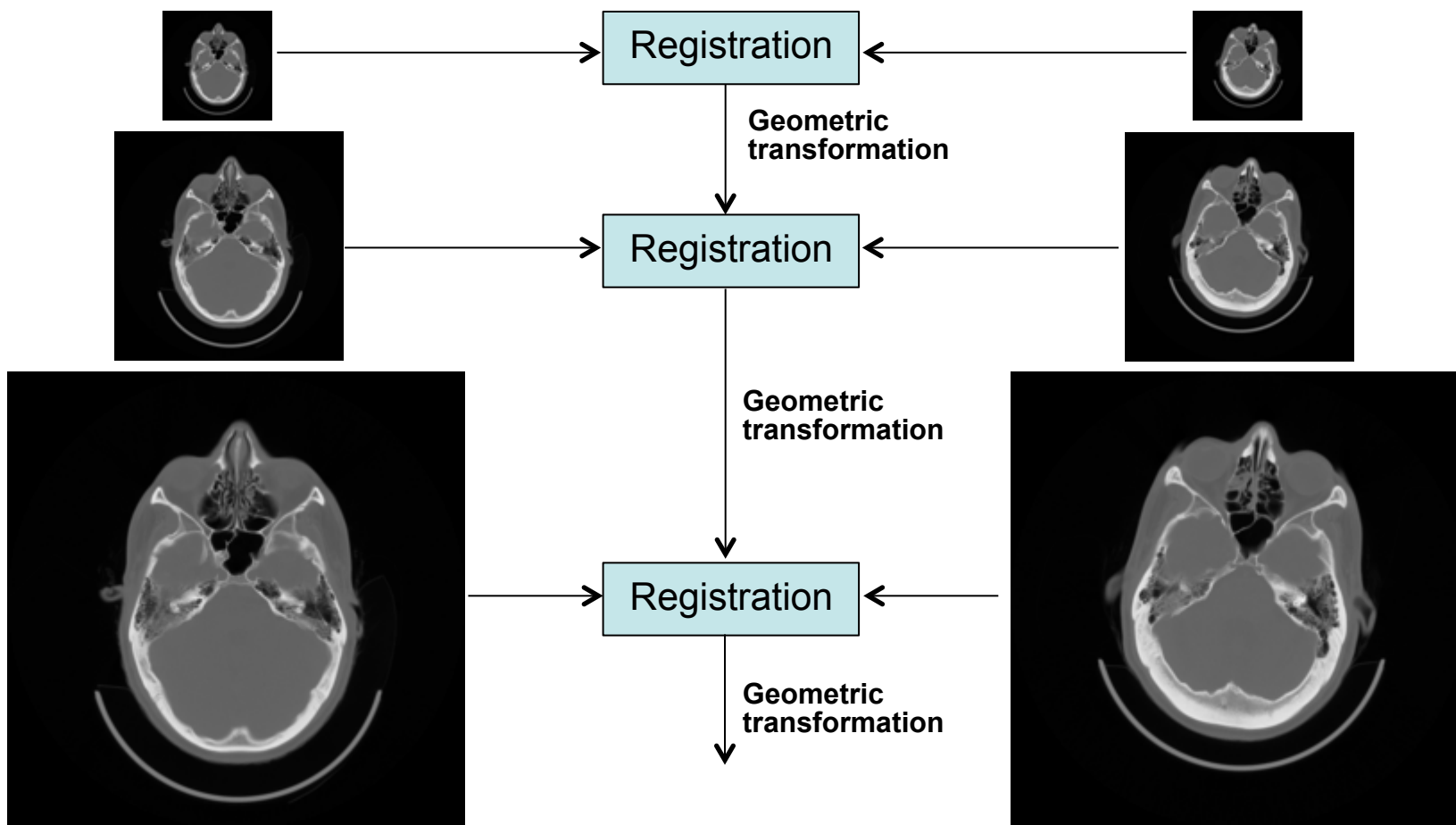


The optimization algorithm stops when a similarity criterion is achieved



Registration based on Iterative Optimization

To speedup the computational process, a **multi-resolution strategy** is frequently used

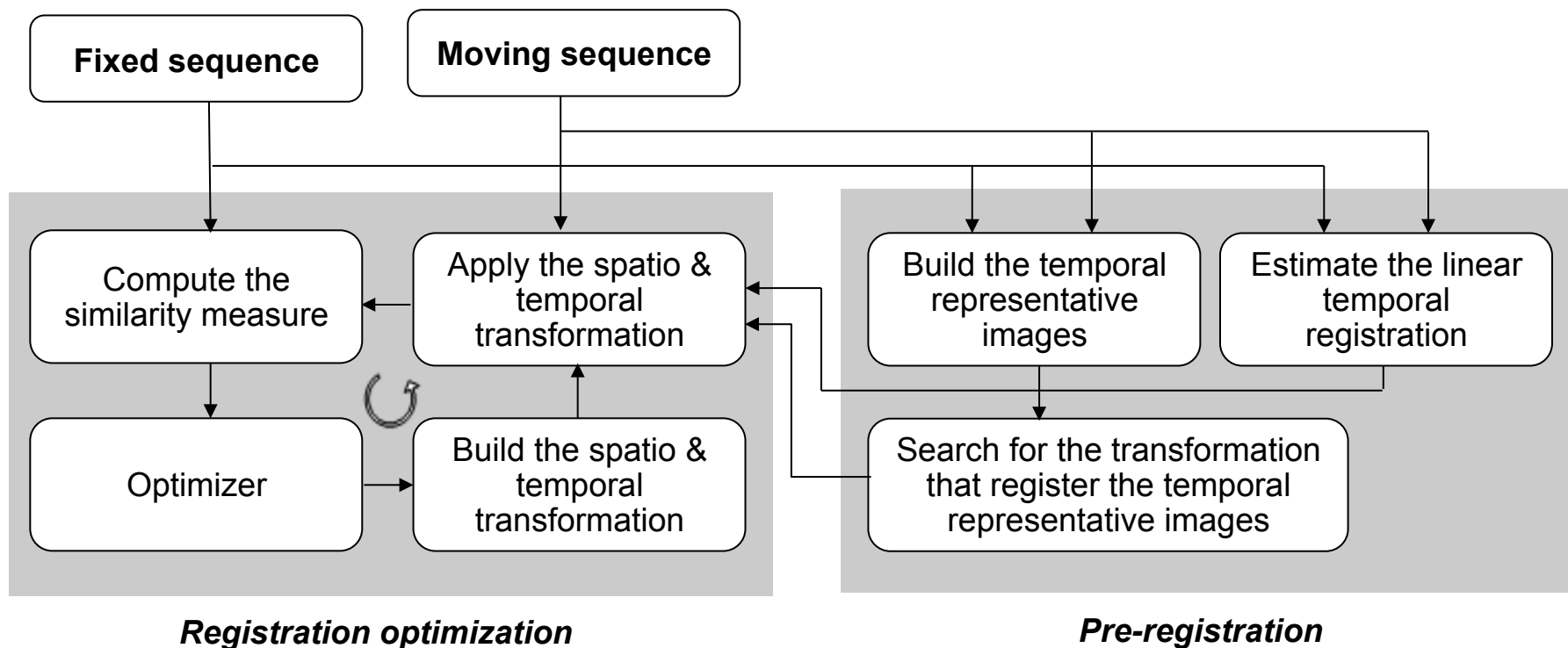




Methods: Spatio & Temporal Registration



Spatio & Temporal registration based on Iterative Optimization



Oliveira, Sousa, Santos, Tavares (2011) *Medical & Biological Engineering & Computing* 49(7):843-850
 Oliveira & Tavares (2013) *Medical & Biological Engineering & Computing* 51(3):267-276



Applications and Results: Plantar Pressure Images



Plantar Pressure Images

A dynamic plantar pressure image sequence represents the **interaction between the foot sole and the ground during a complete step**

Example of a footstep sequence acquired at normal walking speed:



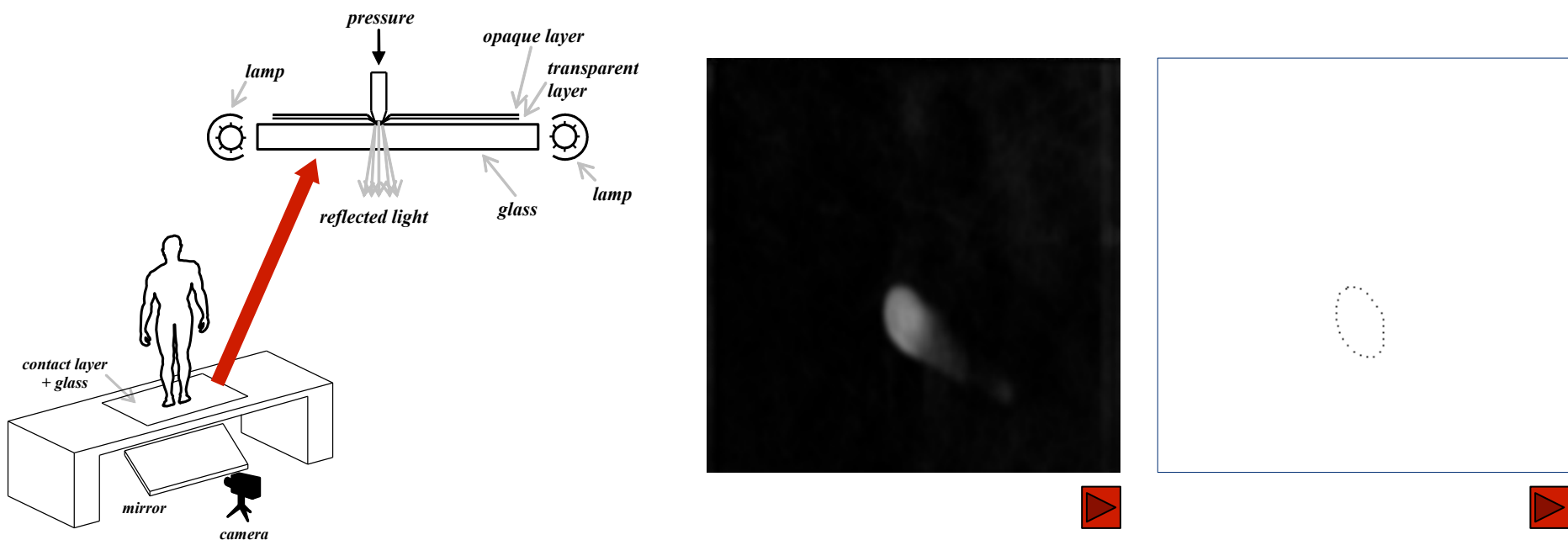
An EMED® plate and an example of an image sequence acquired



Plantar Pressure Images

A dynamic plantar pressure image sequence represents the interaction between the foot sole and the ground during a complete step

Example of a footstep sequence acquired at normal walking speed:



Scheme of a light reflection device and an original image sequence acquired and the corresponding segmented image sequence



Applications of Plantar Pressure Image Analysis

The **automated analysis** of plantar pressure images is **useful in laboratories and clinics**

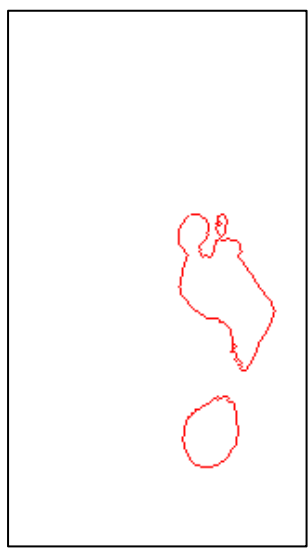
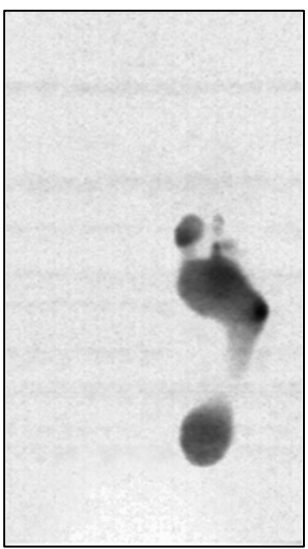
- To facilitate the **automatic computation of several statistical measures** that can be used to study **foot pressure distributions** (e.g. diabetic foot)
- For **building mean plantar pressure images** that are more accurate to represent the pressure distribution than only trial images or image sequences
- To **simplify usual diagnosis tasks**, such as foot classification, foot main regions identification, comparison between feet of different subjects



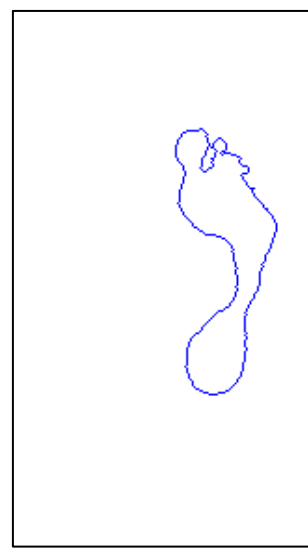
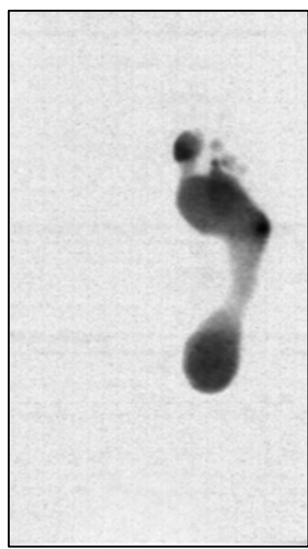
Registration based on Contours Matching

I - Contours extraction and matching

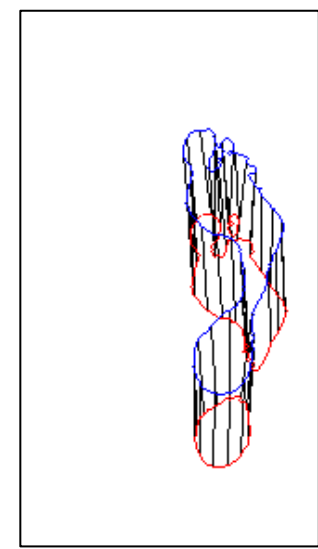
**Fixed image and contour
(optical plantar pressure device)**



**Moving image and contour
(optical plantar pressure device)**



**Matching
established**





Registration based on Contours Matching

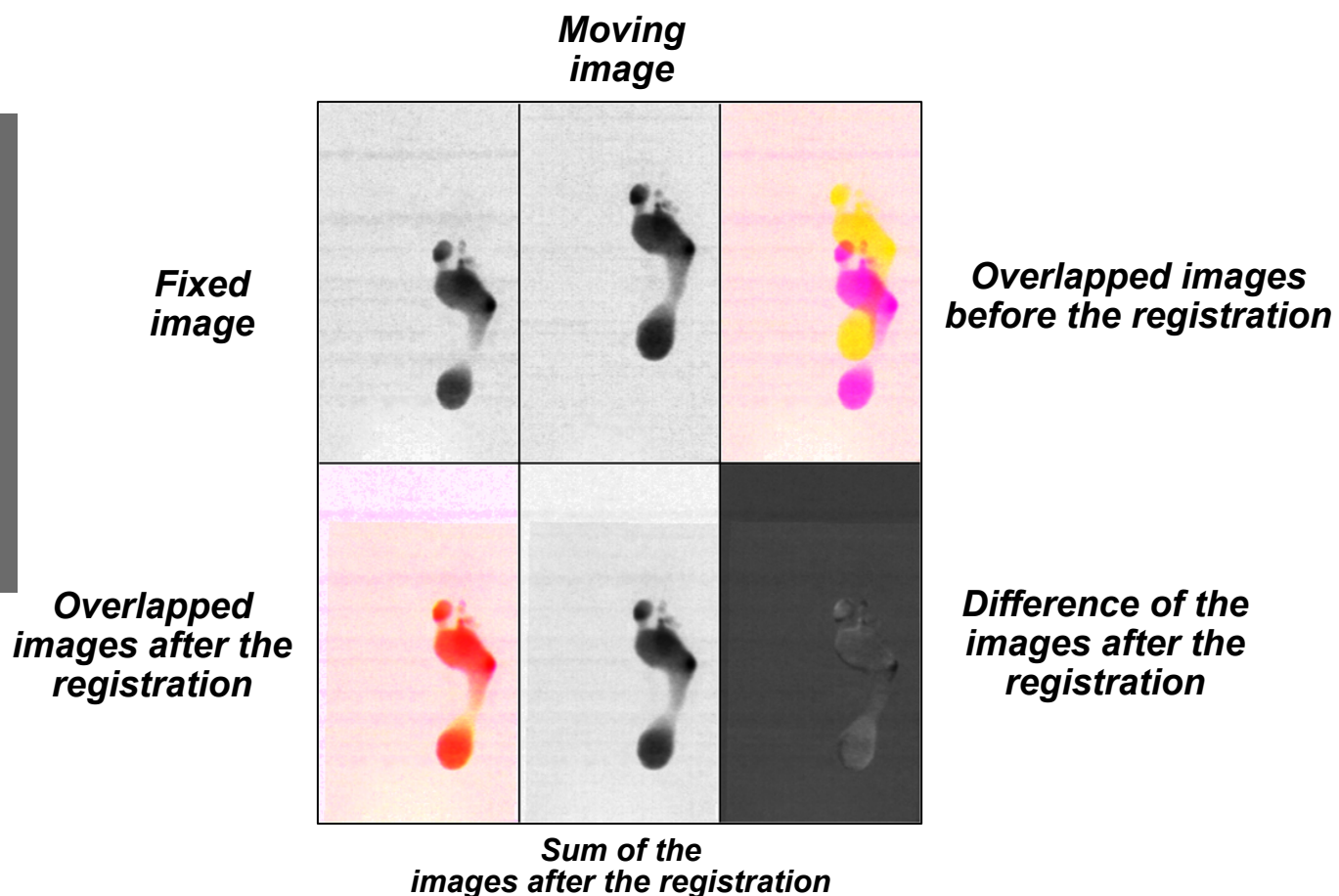
... cont.

II - Registration

Registration: 2D,
monomodal,
intrasubject

Processing time:
0.125 s (AMD
Turion64, 2.0 GHz,
1.0 GB of RAM)

Images dimension:
160x288 pixels





Registration based on Direct Maximization of the Cross-Correlation

Fixed image

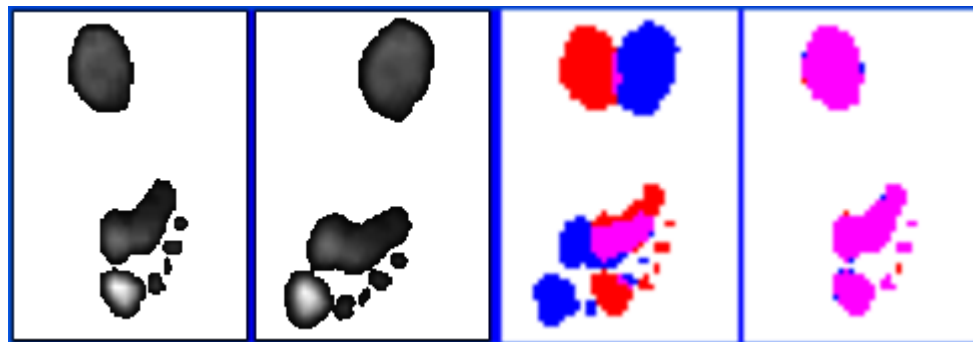
Moving image

Overlapped images before and after the registration

Registration: 2D, monomodal, intrasubject (on the top) and intersubject (on the bottom)

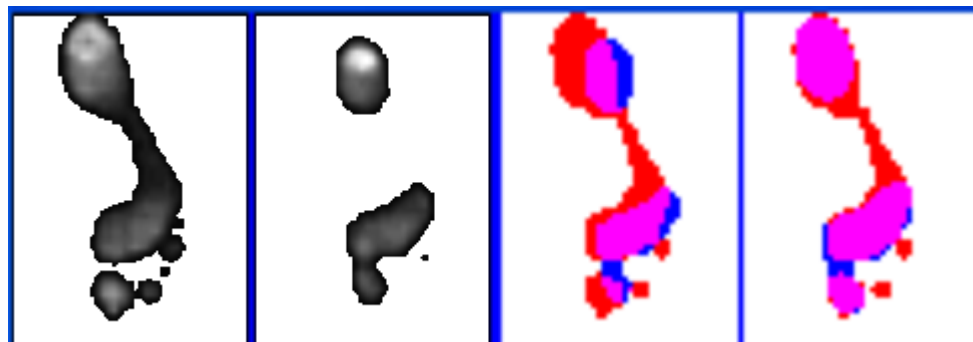
Processing time: 0.04 s (AMD Turion64, 2.0 GHz, 1.0 GB of RAM)

Images dimension: 45x63 pixels



Images from the same foot

Using a rigid transformation



Images from different subjects

Using a similarity transformation



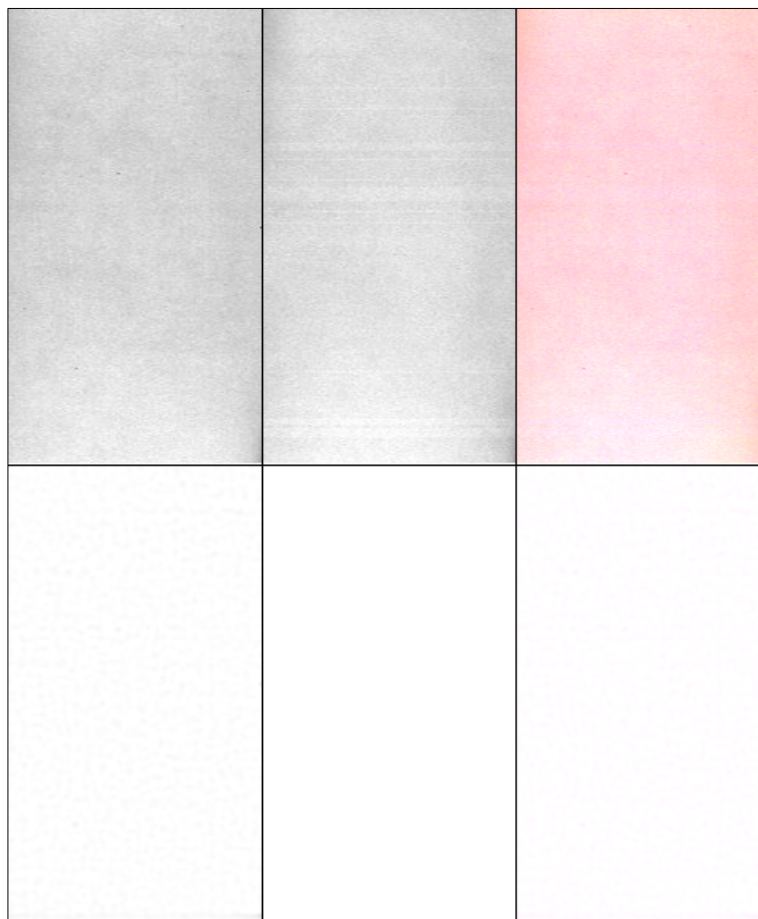
Spatio & Temporal registration of Plantar Pressure Image Sequences

Device: Light reflection
(25 fps, resolution 30 pixels/cm²)

Image similarity
measure: MSD

Sequences dimension:
160x288x22,
160x288x25

Processing time: 1 min
(using an AMD
Turion64, 2.0 GHz, 1.0
GB of RAM)



**Template
sequence**

**Source
sequence**

**Overlapped
sequences**



**Before the
registration**

**After the
registration**



Spatio & Temporal registration of Plantar Pressure Image Sequences

Device: EMED (25
fps, resolution: 2
pixels/cm², images
dimension:
32x55x13; 32x55x18)

Registration: rigid
(spatial), polynomial
(temporal); similarity
measure: MSD

Processing time: 4 s -
AMD Turion64, 2.0
GHz, 1.0 GB of RAM



<i>Fixed sequence</i>	<i>Moving sequence</i>	<i>Overlapped sequences</i>

Before the
registration

After the
registration

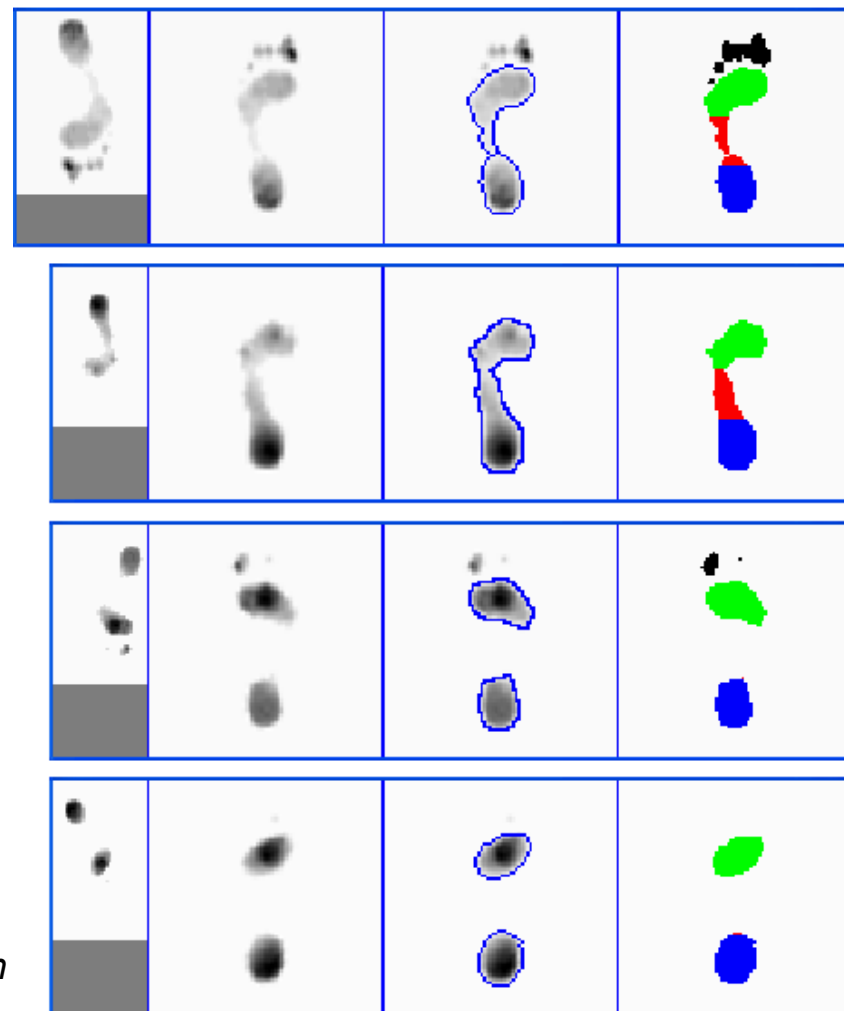




Applications in Plantar Pressure Images Studies

A computational solution has been developed to assist biomechanical studies based on the registration of plantar pressure images, which can be used in:

- Foot segmentation
- Foot classification: left/right, high arched, flat, normal, ...
- Foot axis computation
- Footprint indices computation
- Posterior statistical analysis



Oliveira, Sousa, Santos, Tavares (2012) Computer Methods in Biomechanics and Biomedical Engineering 15(11):1181-1188



Applications and Results: Medical Images



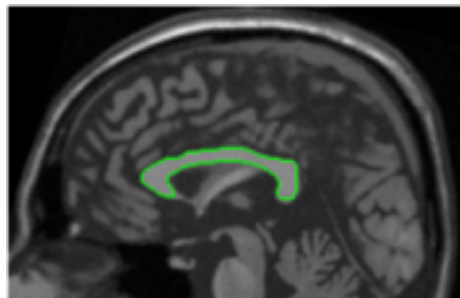
Registration based on Contours Matching

Registration: 2D,
monomodal,
intrasubject

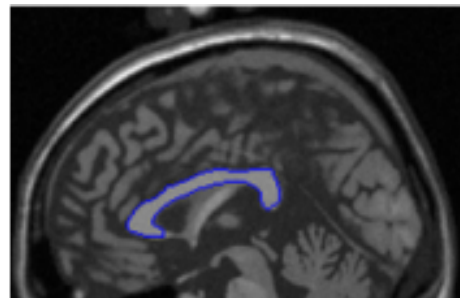
Processing time:
0.5 s (AMD
Turion64, 2.0 GHz,
1.0 GB of RAM)

Images dimension:
217x140 pixels

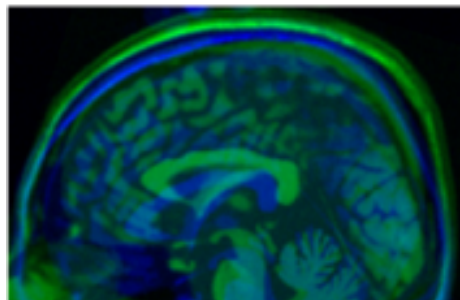
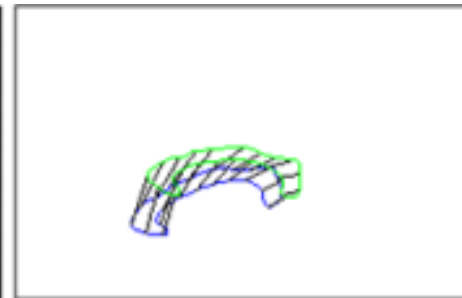
*Fixed image and
contour (MRI)*



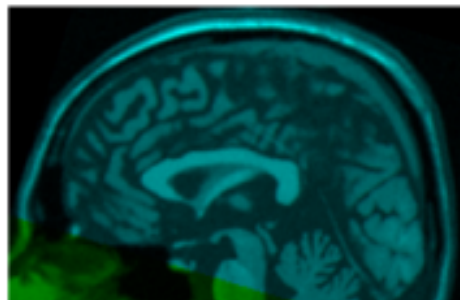
*Moving image and
contour (MRI)*



*Correspondences found
between the Corpus
Callosum contours*



*Overlapped images
before the registration*



*Overlapped images
after the registration*

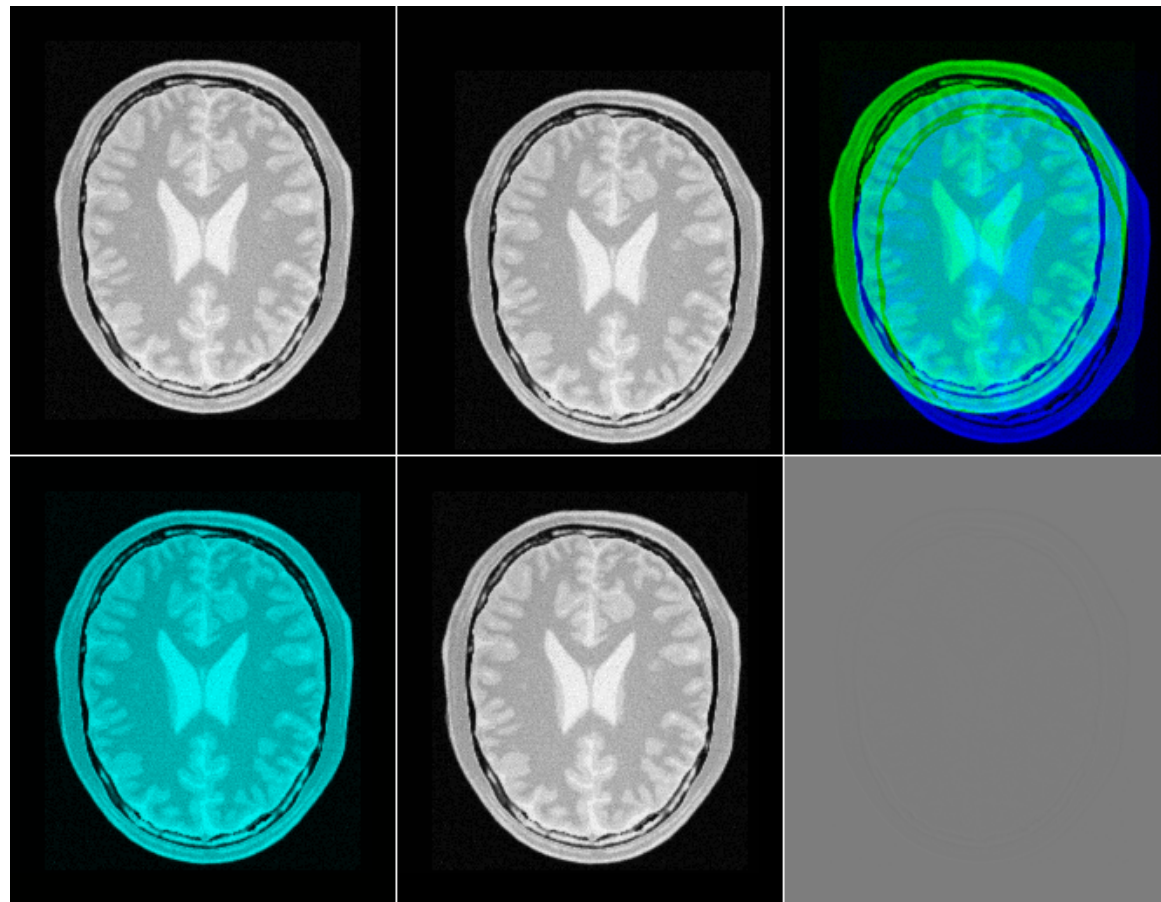


*Difference between the
images after the registration*



Registration based on Fourier transform

Fixed image
MRI (proton density) *Moving image*
MRI (proton density) *Overlapped images*
before the registration



Overlapped images *Sum of the images* *Difference of the images*
after the registration *after the registration* *after the registration*

Registration: 2D,
monomodal,
intrasubject

Processing time: 2.1 s
(AMD Turion64, 2.0
GHz, 1.0 GB of RAM)

Images dimension:
221x257 pixels



Registration based on Iterative Optimization

Registration: 2D,
multimodal,
intrasubject (without
pre-registration)

Similarity measure: MI

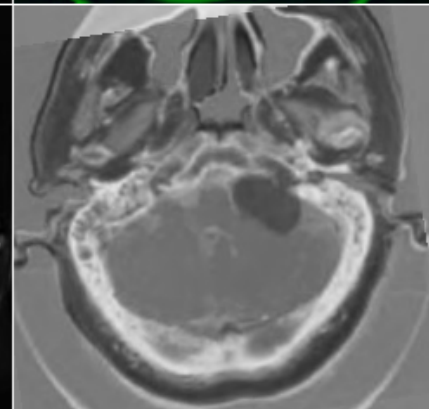
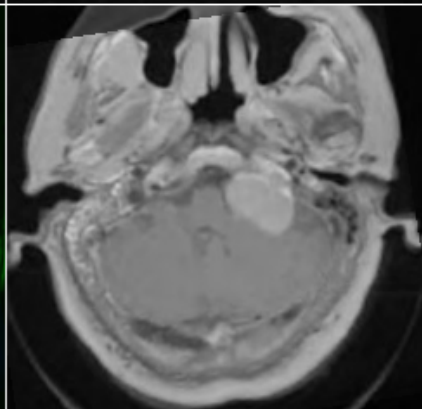
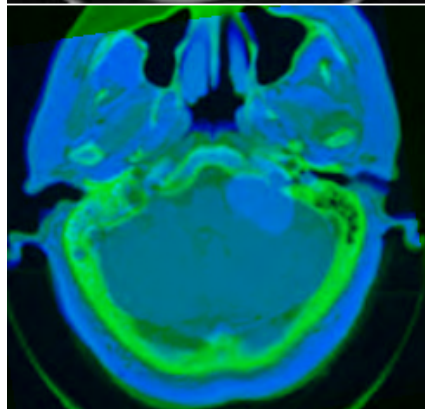
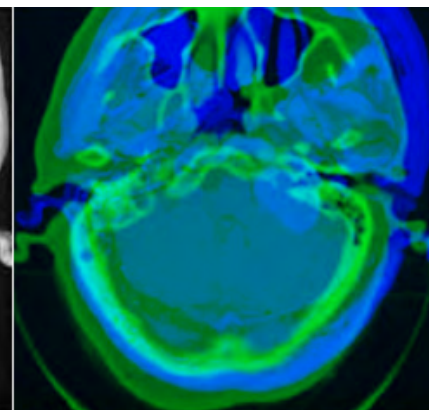
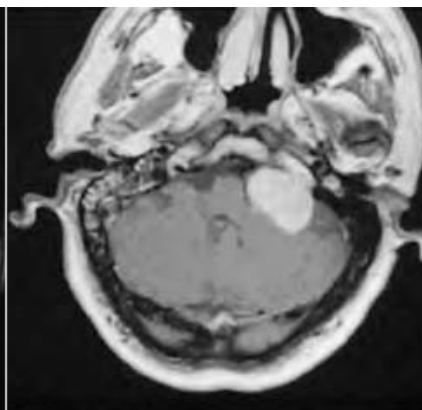
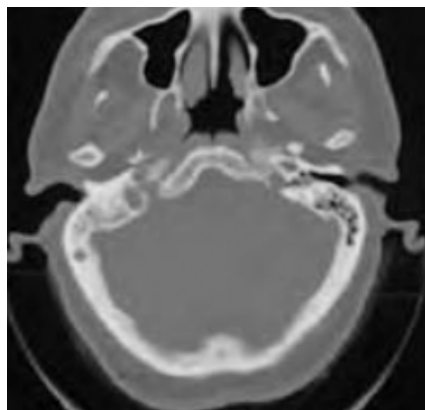
Processing time: 4.6 s
(AMD Turion64, 2.0
GHz, 1.0 GB of RAM)

Images dimension:
246x234 pixels

*Fixed image
(CT)*

*Moving image
(MRI)*

*Overlapped images
before the registration*



*Overlapped images
after the registration*

*Sum of the images
after the registration*

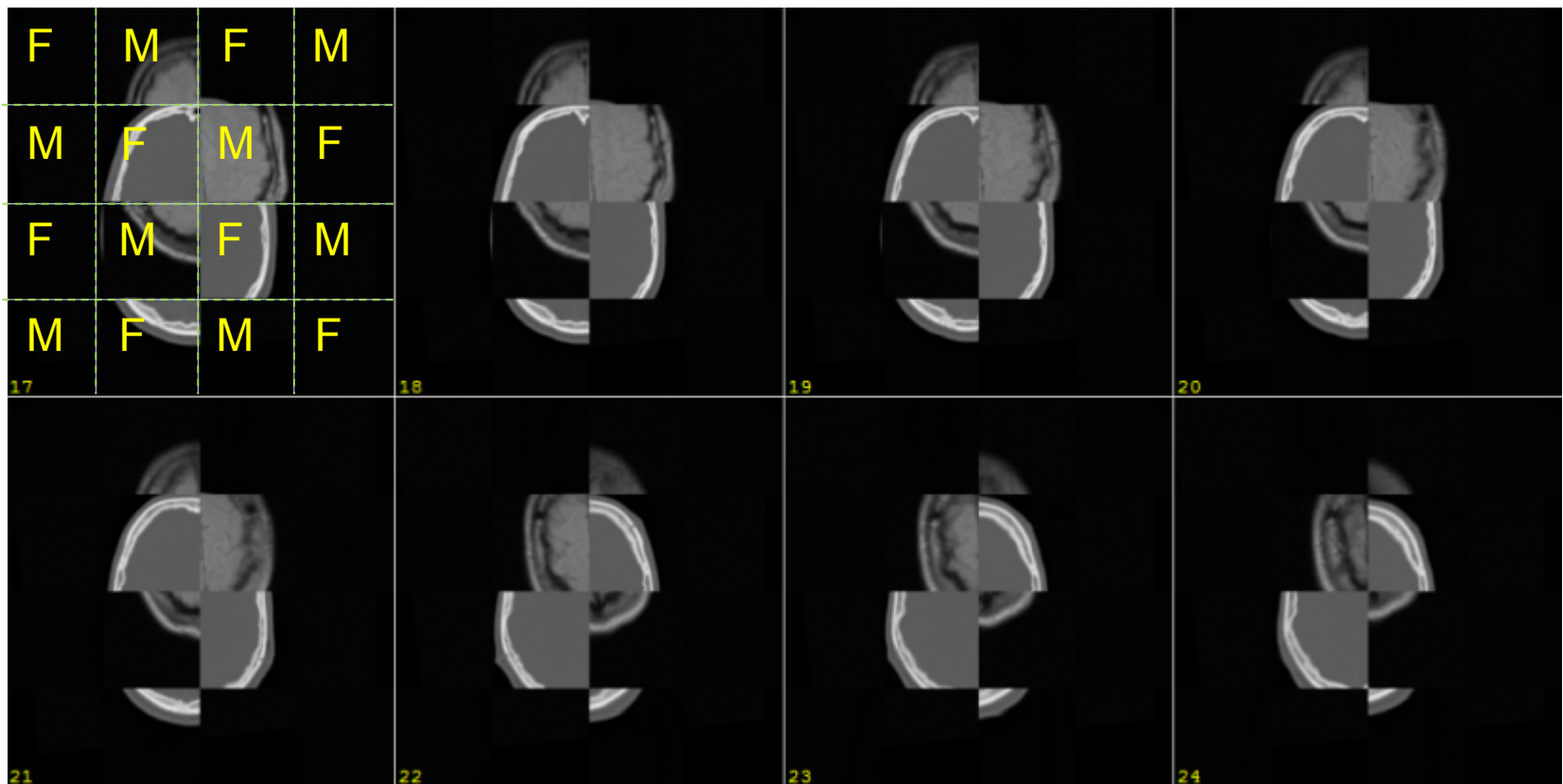
*Difference of the images
after the registration*

Oliveira & Tavares (2014) *Computer Methods in Biomechanics and Biomedical Engineering* 17(2):73-93



Registration based on Iterative Optimization

“Checkerboard” of the slices before the registration (CT/MRI-PD, brain)



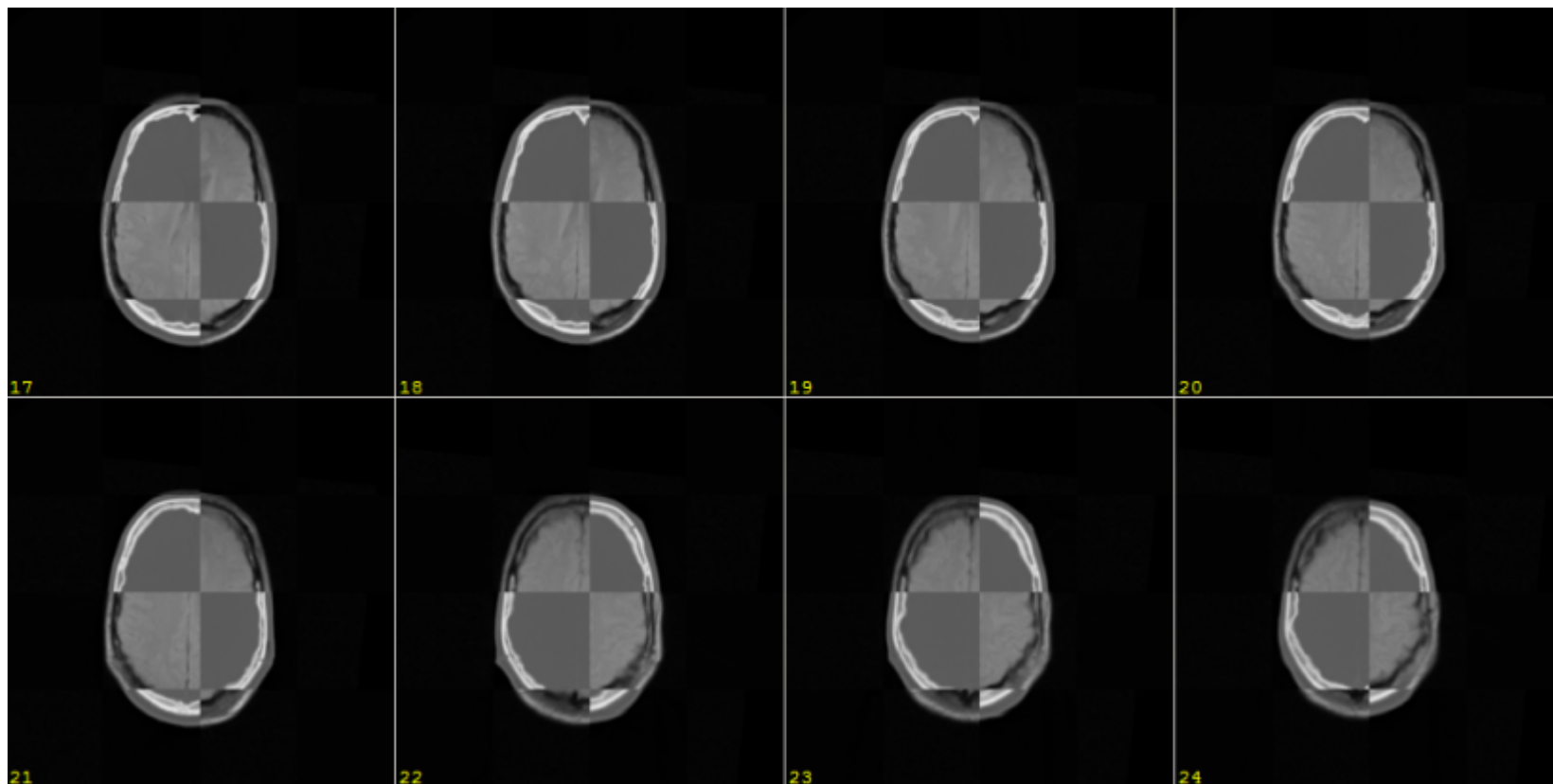
(The “checkerboard” slice is built by interchanging square patches of both slices and preserving their original spatial position in the fixed (F) and moving (M) slices)



Registration based on Iterative Optimization

... cont.

Checkerboard of the slices after the registration (CT/MRI-PD, brain)

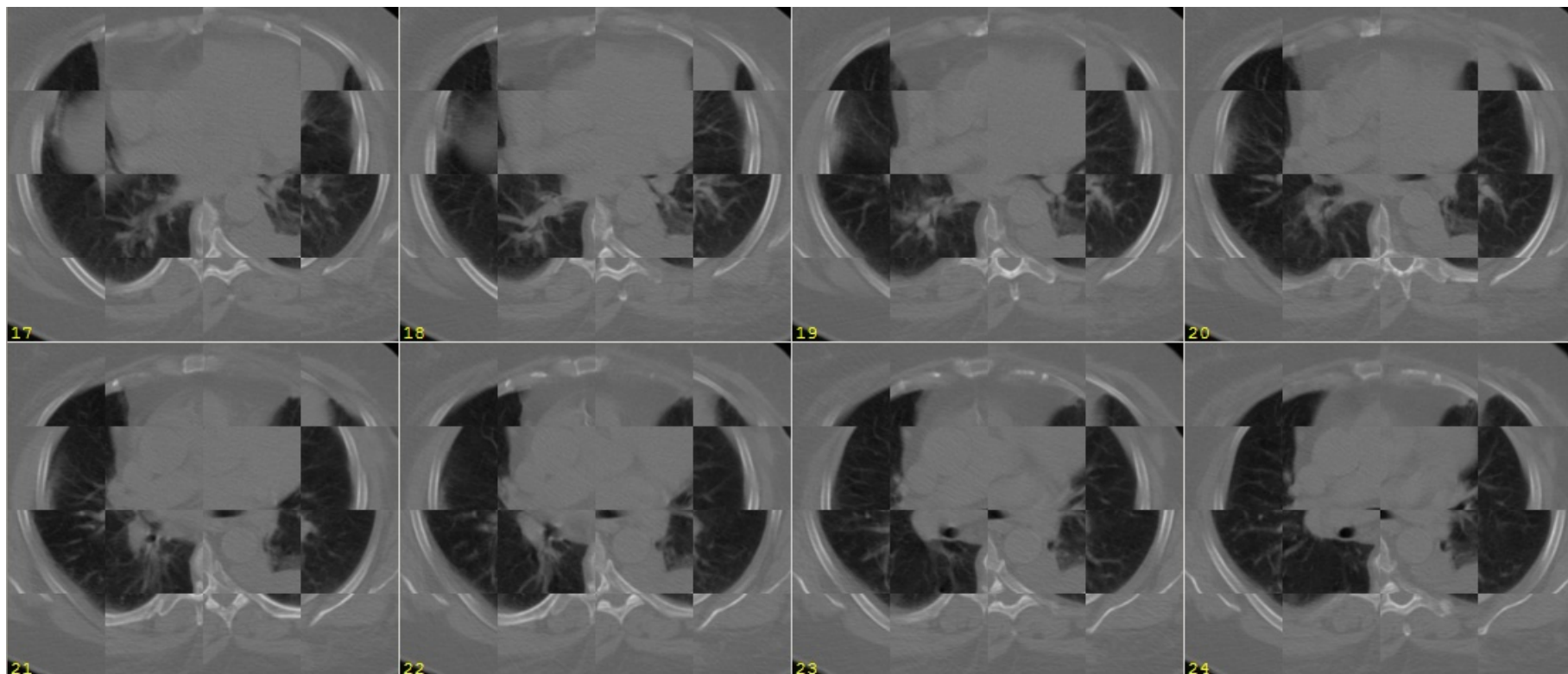


Registration: 3D, multimodal, intrasubject; Similarity measure: MI



Registration based on Iterative Optimization

Checkerboard of the slices (CT, thorax, Δt : 8.5 months) before the registration



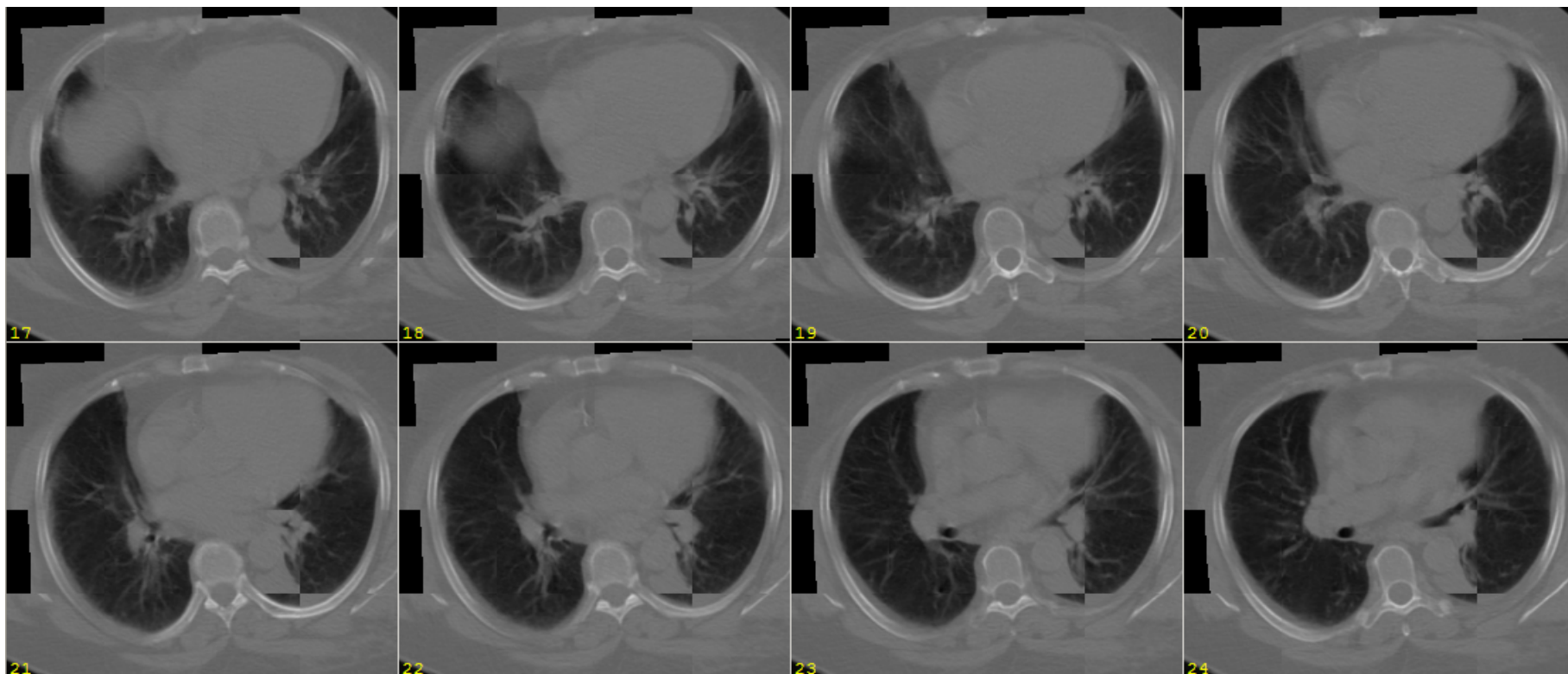
Oliveira & Tavares (2014) Computer Methods in Biomechanics and Biomedical Engineering 17(2):73-93



Registration based on Iterative Optimization

... cont.

Checkerboard of the slices (CT, thorax, Δt : 8.5 months) after the registration



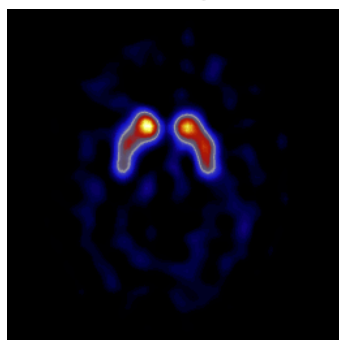
Registration: 3D, monomodal, intrasubject; Similarity measure: MI



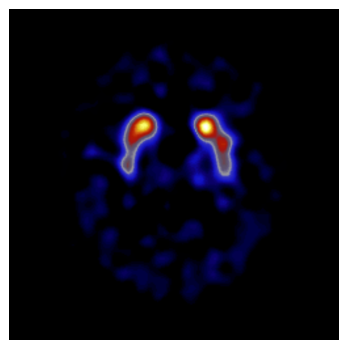
Application in Brain DaTSCAN SPECT images

Brain DaTSCAN SPECT images are used to assist the diagnosis of the Parkinson's disease and to distinguish it from other degenerative diseases. The solution developed is able to:

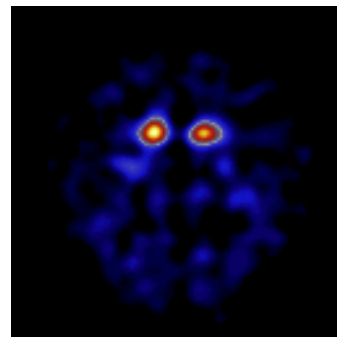
- Segment the relevant areas and perform dimensional analysis
- Quantify the binding potential of the basal ganglia
- Computation of statistical data relatively to a reference population
- Image classification for diagnosis purposes



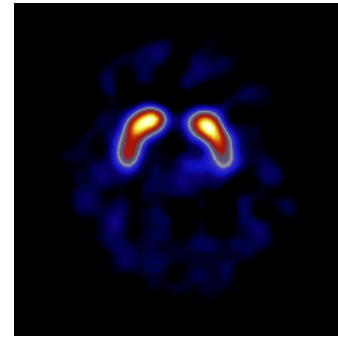
Normal



Alzheimer



*Idiopathic
Parkinsonism*

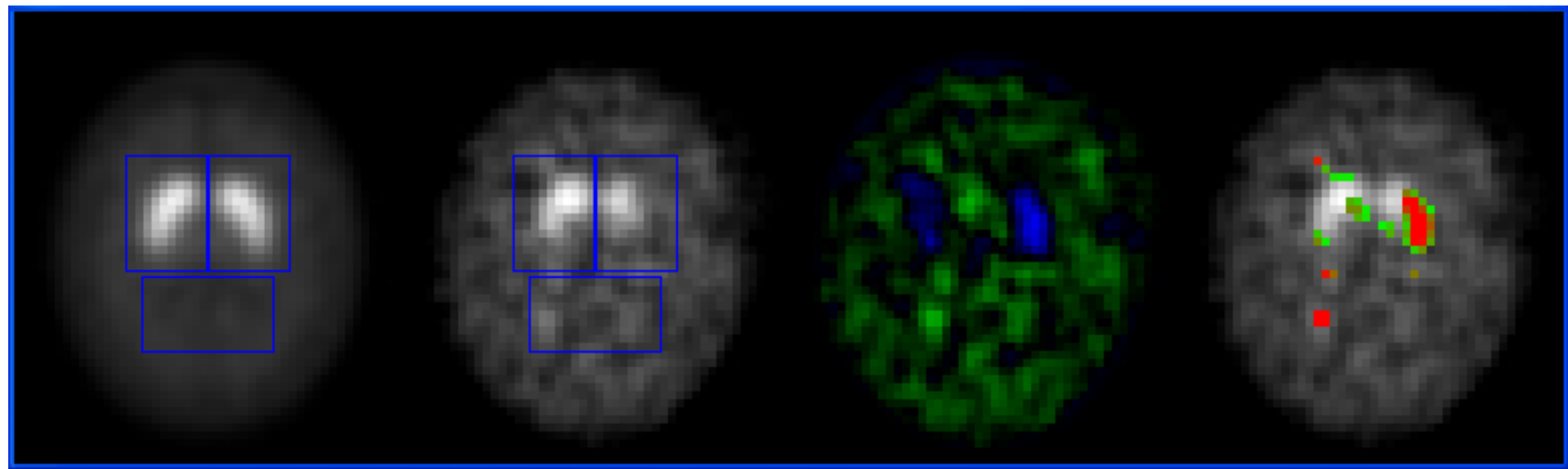


*Essential
tremor*



Application in Brain DaTSCAN SPECT images

3D volume images are automatically registered and statistical analysis relatively to a reference population can be accomplished



Mean slice from the population used as reference

Corresponding slice of a patient

Difference of intensities

Z-scores mapping over the slice (red – high Z-scores)

(The blue rectangles represent the 3D ROIs used to compute the binding potentials)

Oliveira et al. (2014) *The Quarterly Journal of Nuclear Medicine and Molecular Imaging* 58(1):74-84

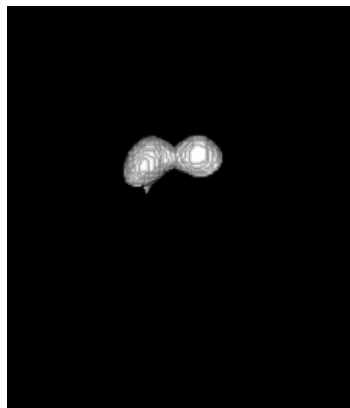


Application in Brain DaTSCAN SPECT images

Basal ganglia 3D shape reconstruction and quantification



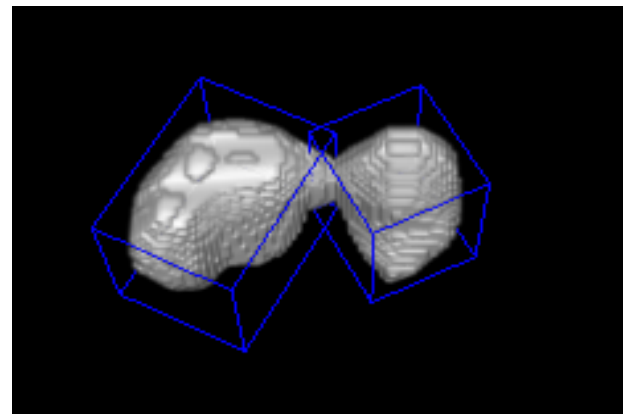
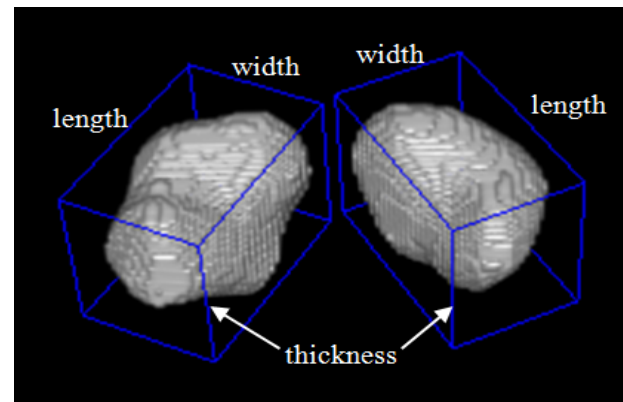
**Basal ganglia
from a mean
image of a normal
population**



**Basal ganglia
from a patient
with idiopathic
Parkinson's disease**



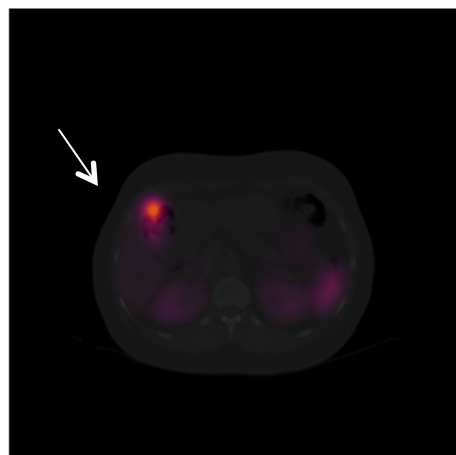
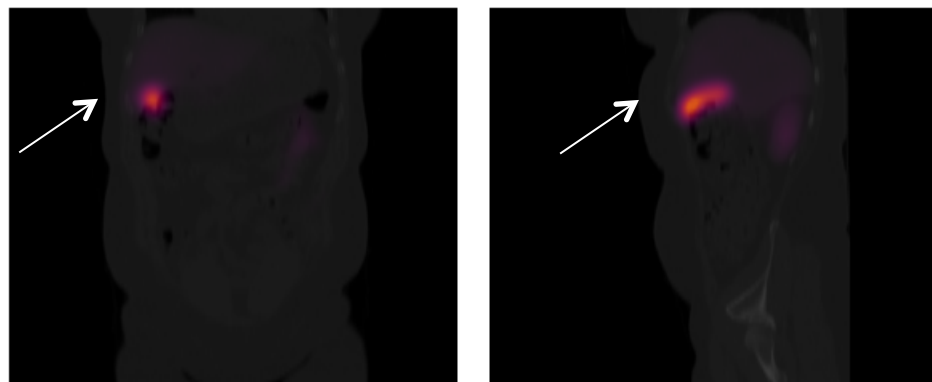
**Basal ganglia
from a patient
with vascular
Parkinson's disease**



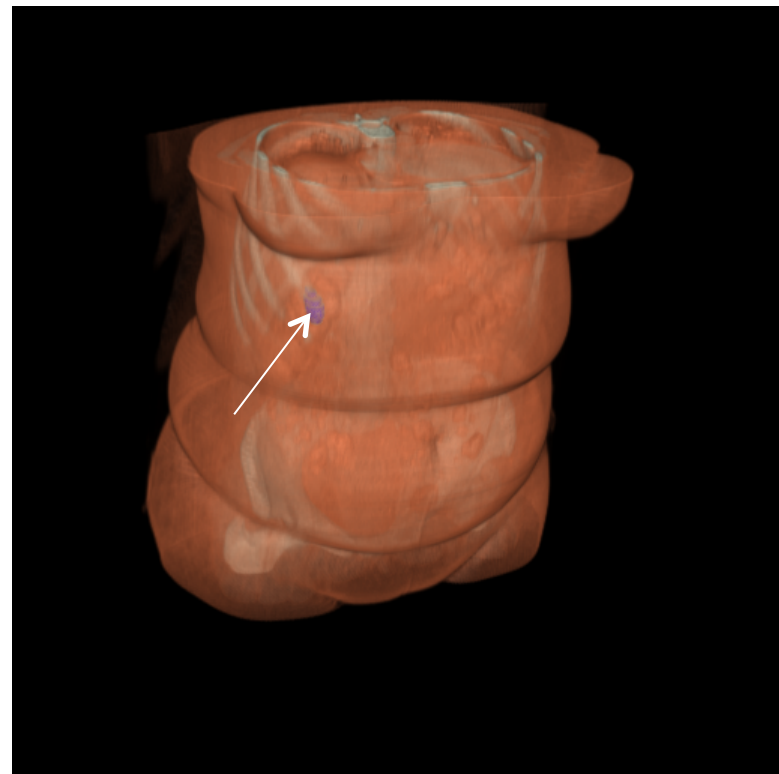
Oliveira et al. (2014) *The Quarterly Journal of Nuclear Medicine and Molecular Imaging* 58(1):74-84



Application in SPECT/CT registration and fusion



Three slices (coronal, sagittal and axial) after registration and identification of the potential lesion

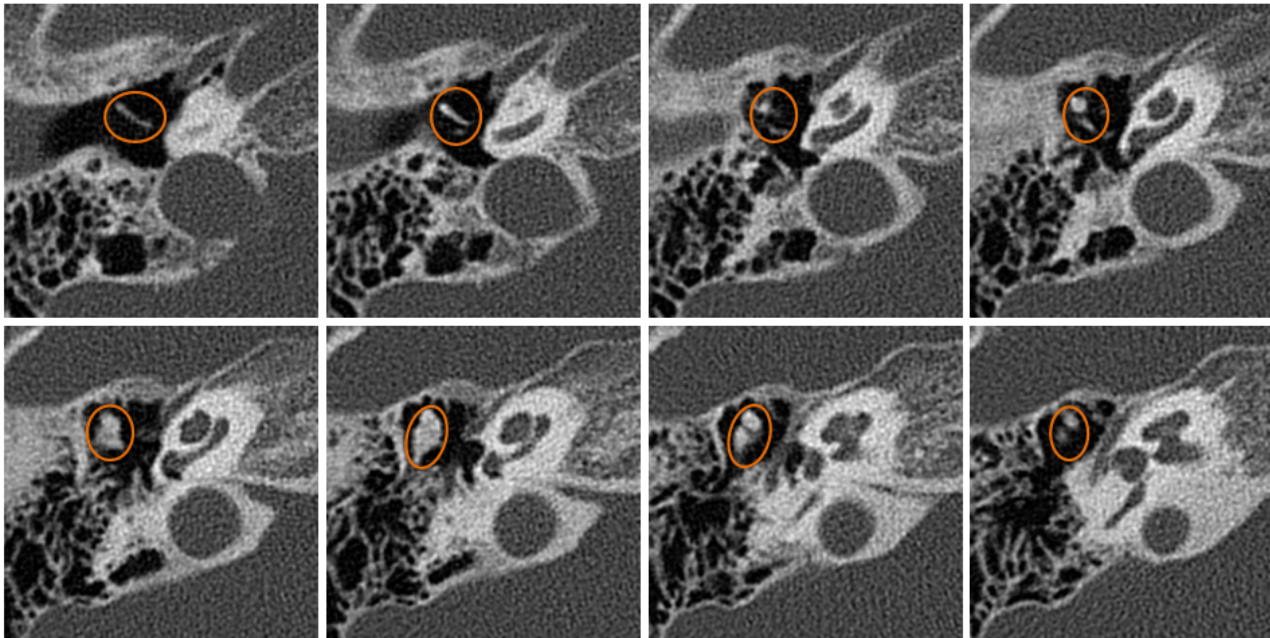


3D visualization after CT/SPECT fusion (the lesion identified in the SPECT slices is indicated)

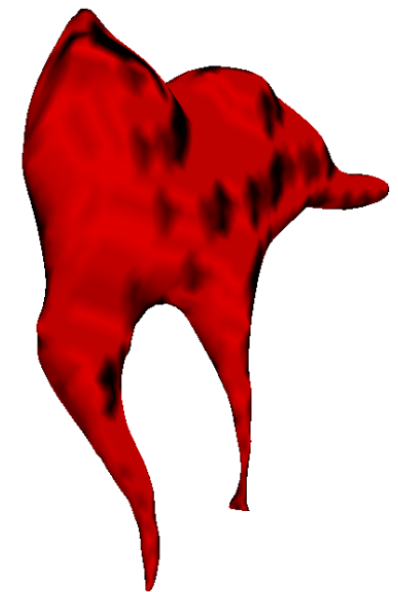


Application in Ear CT images

Application in the fully automated segmentation of the incus and malleus ear ossicles in conventional CT images



TC slices with the incus and malleus ossicles (inside the red ellipse) to be segmented



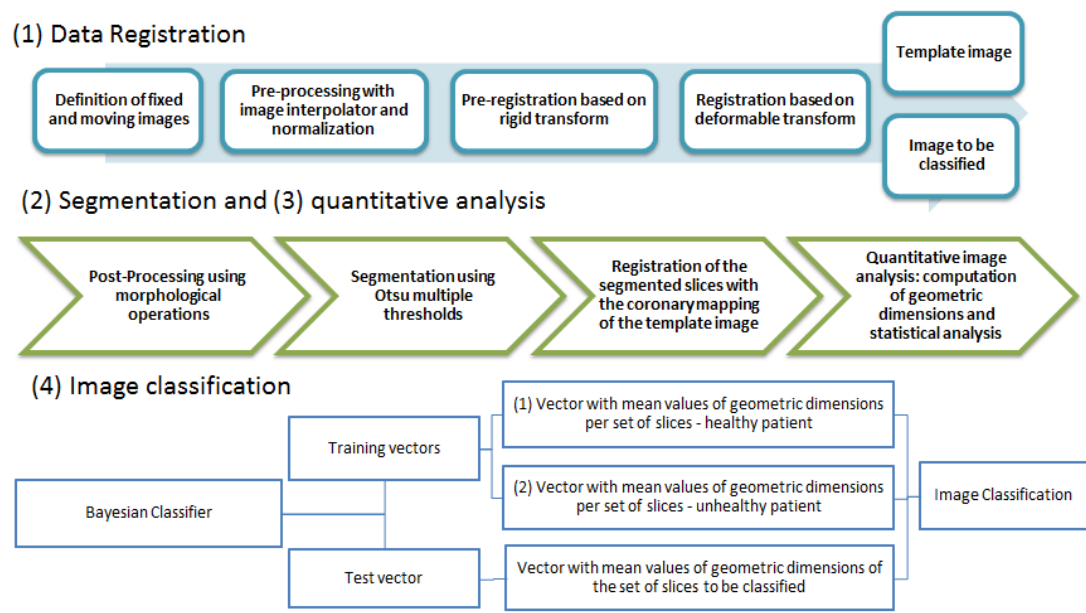
3D surface of the incus and malleus surface built

Oliveira, Faria, Tavares (2014) Proceedings of the Institution of Mechanical Engineers, Part H: Journal of Engineering in Medicine 228(8):810-818, 2014



Application in Gated Myocardial Perfusion SPECT images

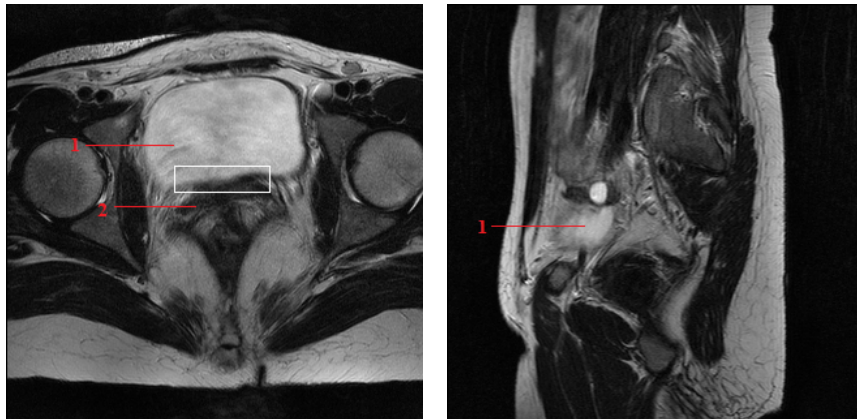
Fully automated segmentation and classification of the images based on image registration and an artificial classifier



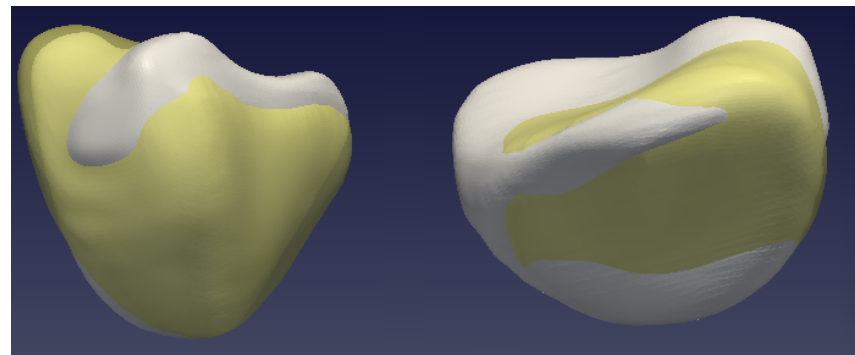
Template image (top), segmented image (bottom-left) and artery mapping (bottom-right)



Application in 3D Reconstruction from multiple views



Axial and sagittal T2-weighted MR images



***3D Reconstruction of the bladder by fusion data
from the axial and sagittal images (2 views)***

Ma et al. (2013) Medical Engineering & Physics 35(12):1819-1824



Conclusions



Conclusions

- **Hard efforts have been made to develop methods more robust and efficient to register images**
- **The Biomedical area has been one of the major promoters for such efforts**; particularly, due to the requirements in terms of low computational times, robustness and of complexity of the structures involved
- We have developed several methods that have been successfully applied in different applications
- **However, several difficulties still to be overcome and better addressed**; such as, severe non-rigidity, complex spatio & temporal behaviors, high differences between the images to be registered (e.g. from very dissimilar image sources), etc.



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Research Team (Computational Vision)



Research Team (Computational Vision)

- Post-Doc students (3):
 - Finished: Alexandre Carvalho
 - In course: Zhen Ma, Simone Prado
- PhD students (14):
 - Finished: Maria Vasconcelos, Zhen Ma, Francisco Oliveira, Teresa Azevedo, Daniel Moura, Sandra Rua
 - In course: João Nunes, Alex Araujo, Carlos Gulo, Roberta Oliveira, Danilo Jodas, Pedro Morais, Andre Pilastrri, Nuno Sousa
- MSc students (31):
 - Finished: Raquel Alves, Carolina Tabuas, Jorge Pereira, Luis Ribeiro, Luis Ferro, Rita Teixeira, Liliana Azevedo, Diana Cidre, Célia Cruz, Priscila Alves, Pedro Gomes, Nuno Sousa, Diogo Faria, Elisa Barroso, Ana Jesus, Frederico Jacobs, Gabriela Queirós, Daniela Sousa, Francisco Oliveira, Teresa Azevedo, Maria Vasconcelos, Raquel Pinho, Luísa Bastos, Cândida Coelho, Jorge Gonçalves
 - In course: André Silva, Silva Bessa, André Costa, João Ribeirinho, Frederico Junqueira, Ricardo Lé
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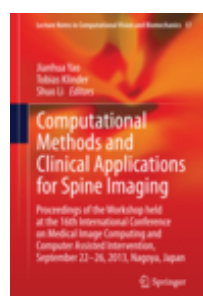
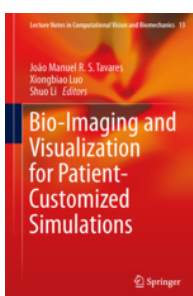
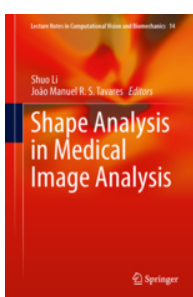
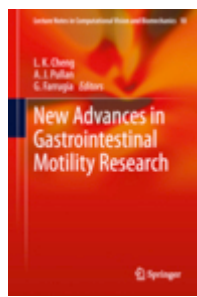
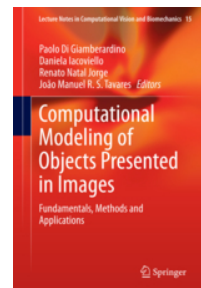
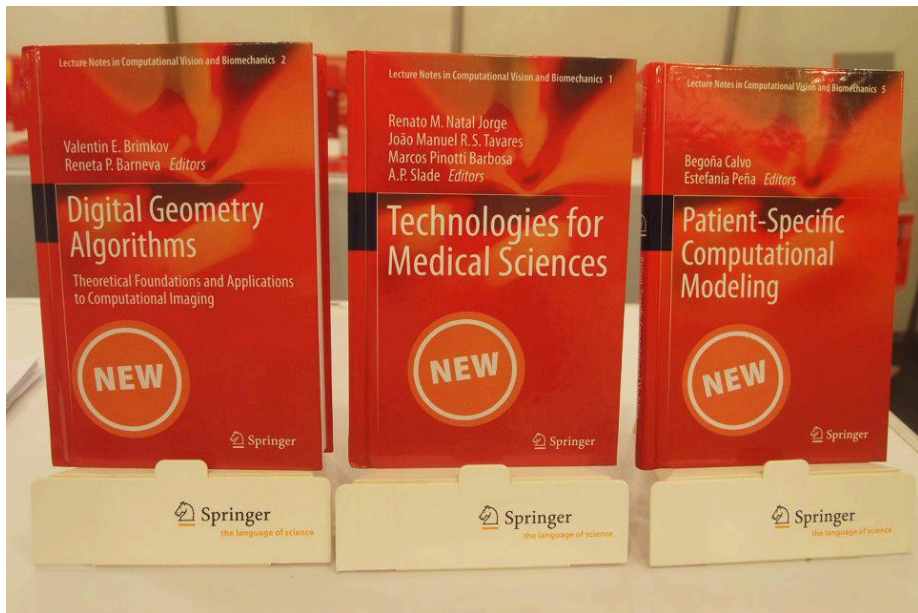
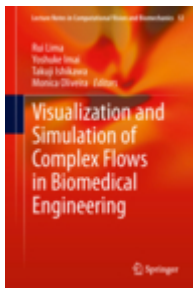
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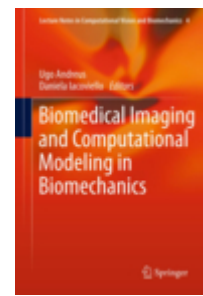
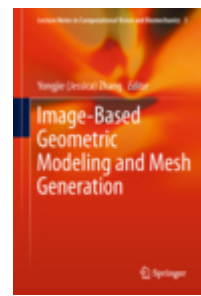


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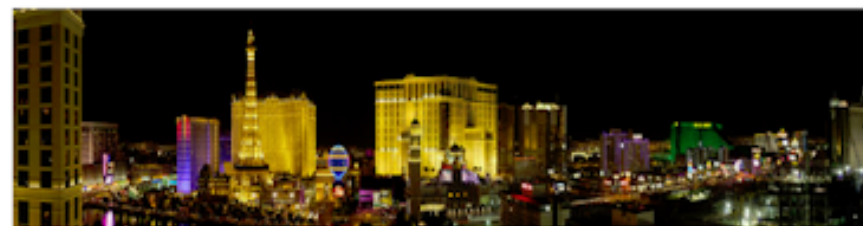


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FEUP Faculdade de Engenharia

João Manuel R. S. Tavares
Associate Professor
FEUP - DEMec

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