



# APPLIED SIGNAL AND IMAGE PROCESSING RESEARCH FOR HEALTHCARE: THE INOVA+ EXPERIENCE

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## COMPANY PROFILE



**INOVA+** is a Portuguese consultancy firm founded in 1997 with headquarters in Oporto and offices in Lisbon specialized in **innovation management**.

As the Portuguese leader in the **promotion and management of European funded projects**, **INOVA+** has a vast experience in the field both as partner and as co-ordinator.

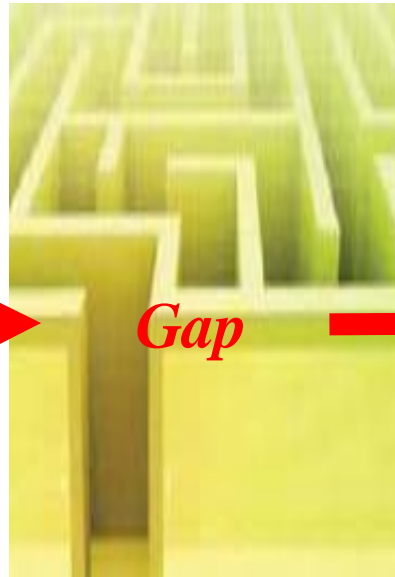
It is connected to the **INNOVA Group** the **largest private network for innovation services in Europe** with offices in Portugal, Italy, Belgium, Luxembourg, France, Poland, Czech Republic and USA.

Promoting **entrepreneurship** and **technology transfer** by matching research results with the market demand.

## UNIVERSITY (Science)



*Gap*



## Market





To be the innovation partner of a larger number of companies



To be the Technology Transfer partner of a bigger number of Universities and S&T centres



To be recognised in Portugal and in Europe as a reference in innovation



To be a preferred link to other european organizations





PROJECTS



# PROJECTS

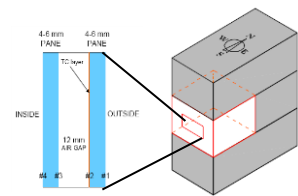
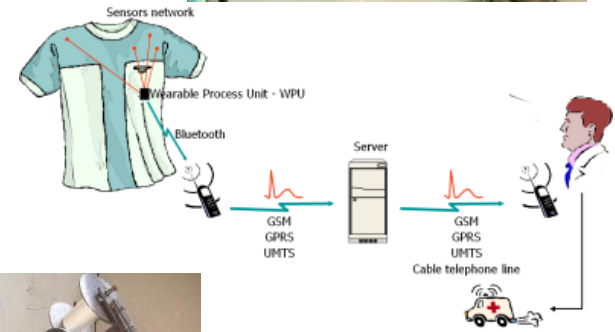
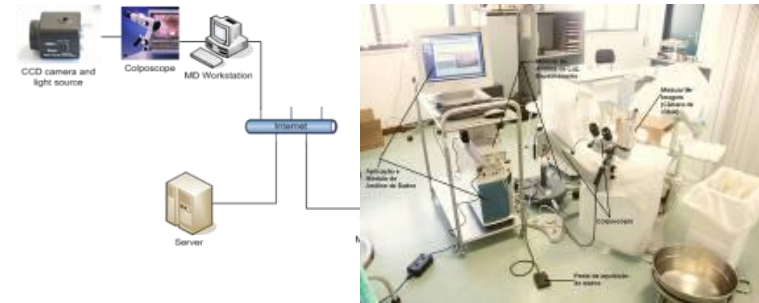
Lifelinger & Cervicare– A new ICT-Based Diagnosis Procedure and Tool set for Early Detection of Cervix Cancer – image processing, spectrometry, neural networks, data-mining, Electronic record.

ADAPT - Automatic Data Transfer (paper, EDI, Fax...to ERP) – XML, OCR, BD

Heartronic – Prevention and early warning of cardiovascular anomalies – telemetry, embedded systems, neural networks

Multiweave – Weaving Machine for Producing Multiaxial Fabric – engineering, HW/SW control

Termoglaze – Production of thermochromic glazing for energy saving applications – simulation using mathematic models to optimize the glazing layers





# PROJECTS

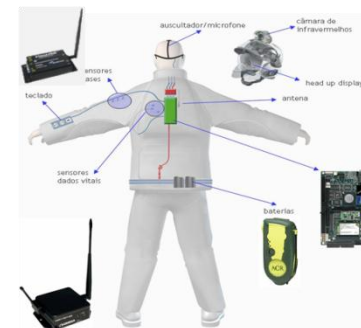
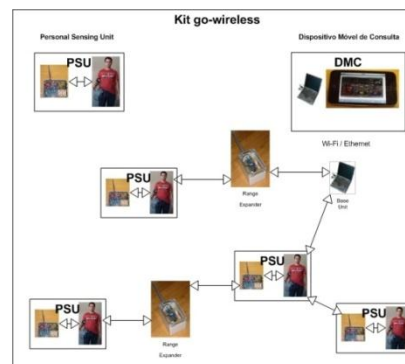
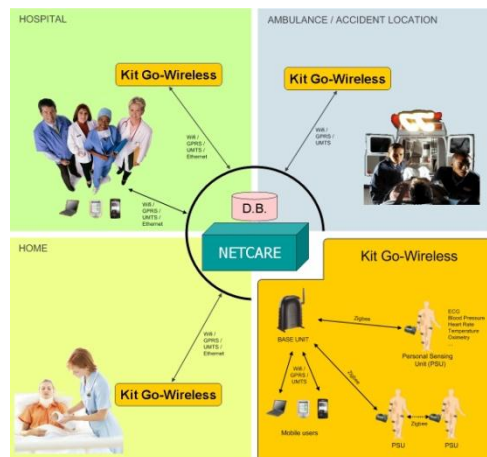
**NETCARE** – Wireless telemetry for continuous health care – telemetry, embedded systems, bio-sensors, zigbee, universal gateway, Zephir integration, Hospital Information System, automatic alarms

**Healththreats** – Integrated Decision Support System for HEALTH THREATS and crises management (Sep/2010) – DSS, workflow

**MAP** – Microchip Analyzer of Proteins (Feb/2011) – data acquisition, analysis software

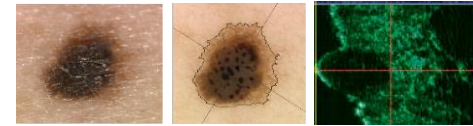
**PHN** - Personal Healthcare Networks (Aug/2011) - telemetry, embedded systems, bio-sensors, zigbee, universal gateway, automatic alarms, GIS

**FIERCE** - Future technologies for first responders in critical infrastructures (Aug/2011) - embedded systems, wireless sensors, zigbee, universal gateway, automatic alarms, GIS



## PROJECTS

SkinMonitor – Diagnosis of skin cancer based on ICT tools –digital imaging, narrow band imaging, ultrasounds



NFCE – New functionalities for the endoscopic capsule – Automatic Diagnosis, spectrometry, Capsule movement control



PRK\_TREATMENT - Exercise System for Parkinson continuous treatment and rehabilitation



AAL4ALL - Standard of Primary Care for AAL services



TICE.Healthy – Health and Life Quality Systems



# troy

Endoscope Capsule Using Ultrasound Technology

TROY PROJECT

Please Check the Video at:

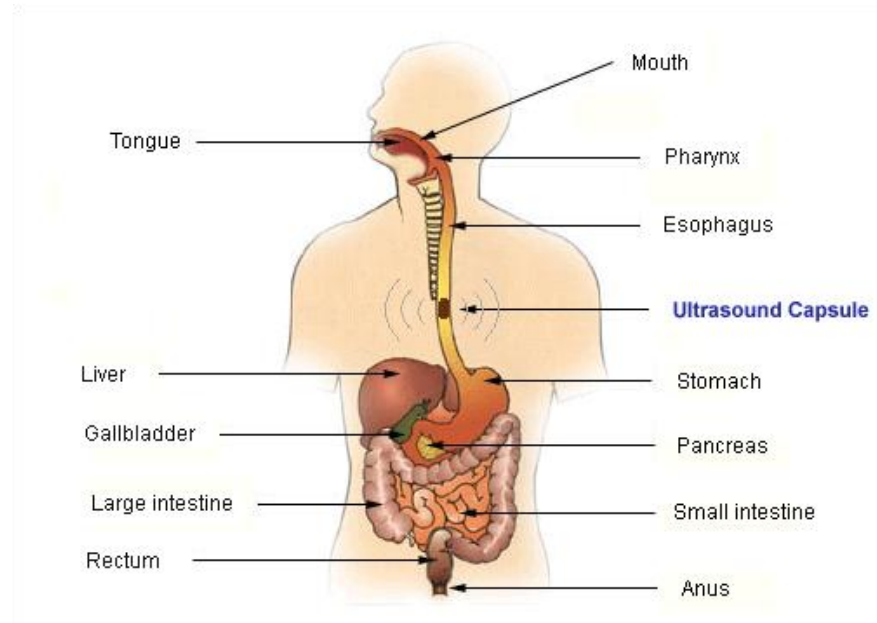
<http://www.inovacao.net/troy/VideoTroy.swf>

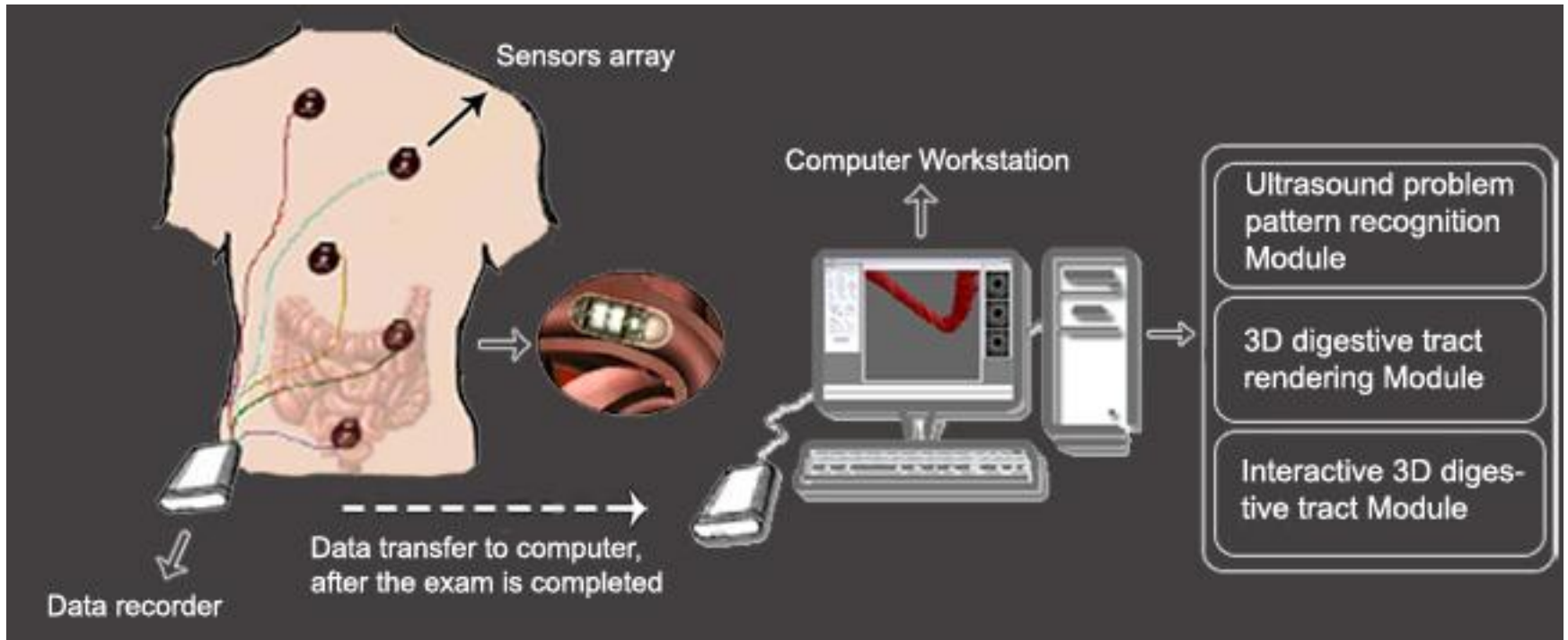
Drink it with a glass of water

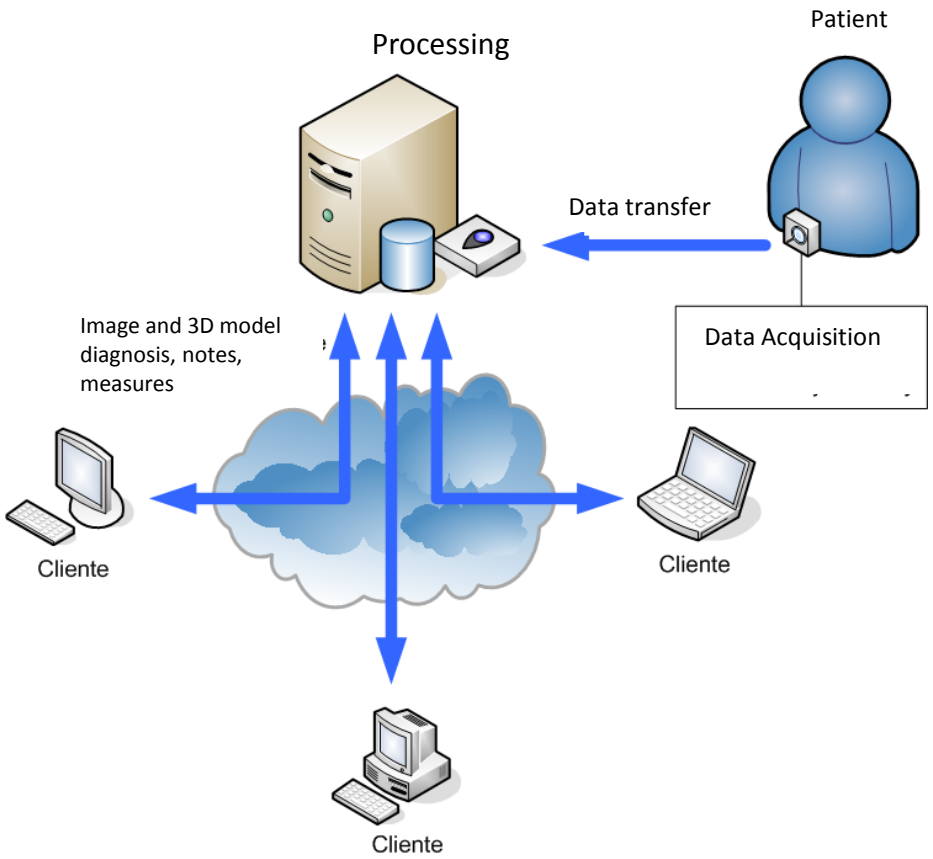
Do your normal life

Return the data logger

Get the results







- Processing Server

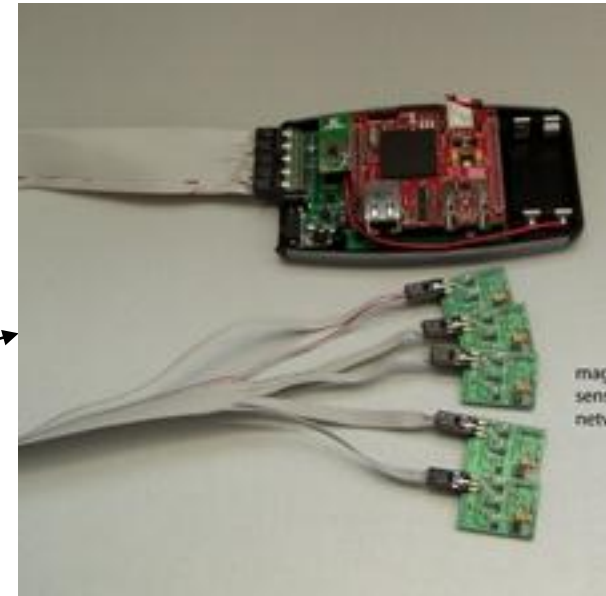
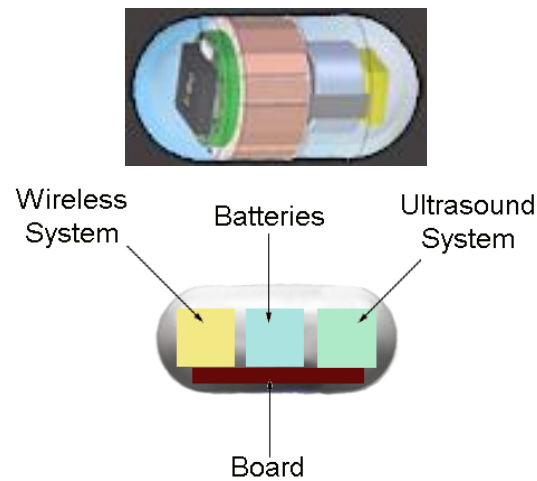
- Process
- Storage
- Simple Interface

- Clients

- Data Access
- Complex Interface 3D Model

## Capsule Architecture

Capsule localization system based in Magnets

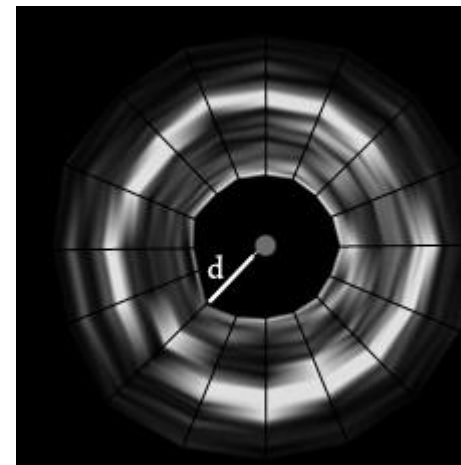
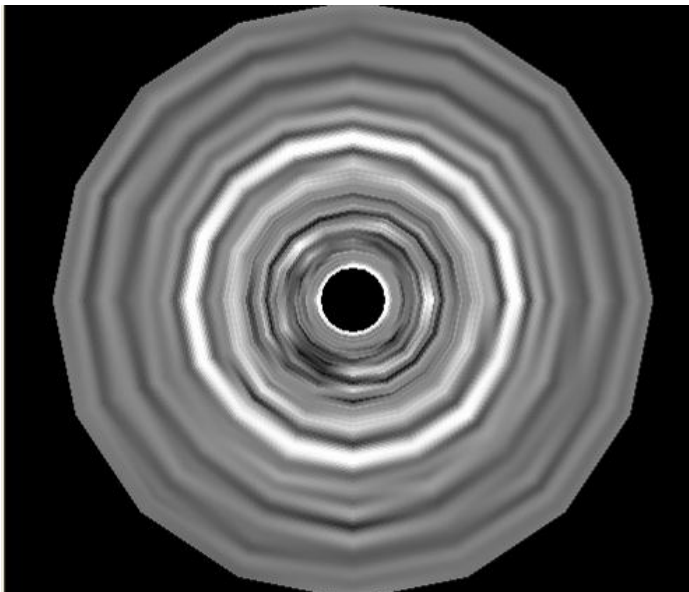
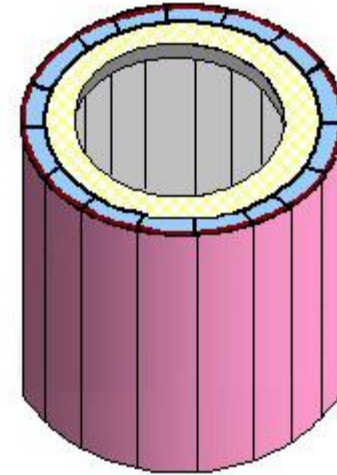




## Pre-Processing (2D images)

2D image from ultrasound raw data

- The objective is to transform the
- 2D ultrasound data in 2D images.
- The capsule is composed of 16 / 32 sensors.
- Each sensor sends an ultrasound signal.



## Pre-Processing (2D Images)

### Metadata on images

Image, position, orientation, rotation and time

```
# filename pos_x pos_y pos_z orient_x orient_y orient_z rotation time
.\Screen0000.bmp -10,000 -50,000 50,000 0,000 1,000 0,000 0,000 0
.\Screen0001.bmp -9,963 -47,713 49,917 0,016 1,000 -0,018 0,000 1
.\Screen0002.bmp -9,855 -45,356 49,674 0,032 0,999 -0,036 0,000 2
.\Screen0003.bmp -9,679 -42,934 49,279 0,047 0,997 -0,053 0,000 3
...
```

Test data was created based on ultra-sound images collected

## Troy capsule data

Position, orientation, rotation, time, Raw data 16 sensors

**Position, pos\_x, pos\_y, pos\_z, Acceleration, orient\_x, orient\_y, orient\_z, rotation, time, Sensor 0 , 3000 values, Sensor 1, ..., Sensor 15, 3000 values**

Position,0,0,0,Acceleration,16567,64954,64314,Sensor n. 0,0,0,2075,2076,2074,2072,2074,2071,2072,2062,3842,4054,...  
Position,0,0,0,Acceleration,16547,64973,64372,Sensor n. 0,0,0,2072,2072,2070,2070,2069,2066,2064,2061,2141,3820,...  
Position,0,0,0,Acceleration,16564,64808,64424,Sensor n. 0,0,0,2060,2058,2060,2062,2062,2063,2065,2066,3825,3810,...  
Position,0,0,0,Acceleration,16570,64912,64352,Sensor n. 0,0,0,2043,2044,2046,2047,2046,2046,2048,2051,3836,3798,...

...

Test data collected at Roma

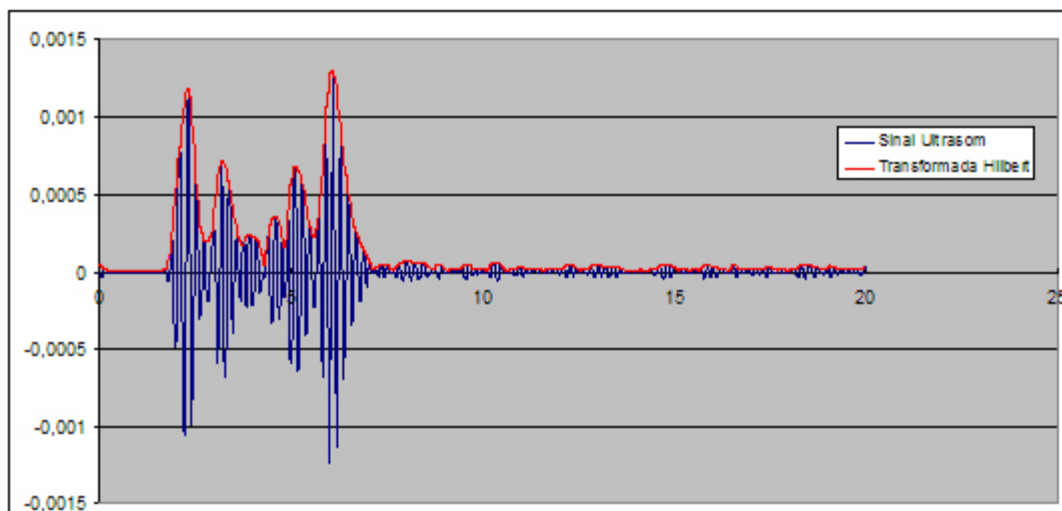
### 2D image from ultrasound raw data based on several consecutive slices

1. Hilbert transform applied to the calibrated signals;
2. Calculate maximums choosing them accordingly with MODA of X signals; MODA of the number of local "maximums" (contours)
3. Make mean and standard deviation of time and amplitude and exclude signals outside standard deviation; this is for signals not excluded in step before.
4. Calculate mean of valid maximums obtaining the contours.
5. Use the values of the fragment closer to the mean to apply the color.

## Hilbert Transform Step

Signal is processed into the Hilbert transform.

This transform creates an envelope around the signal which facilitates identification and analysis of the peaks of the oscillations.



## Signal analysis Step 1/3

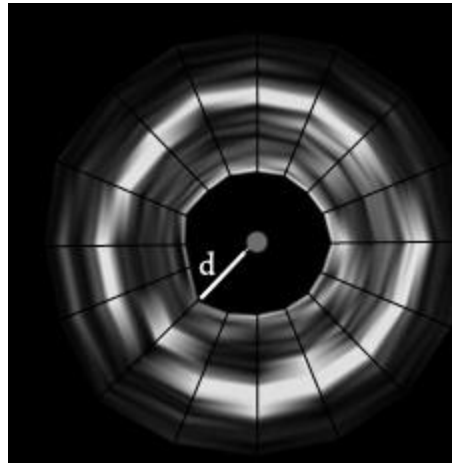
Calculating the distance to the center of the dish:

The contour is calculated using the formula:

$$d = t * 0.75$$

t is the instant of maximum time in millisecond

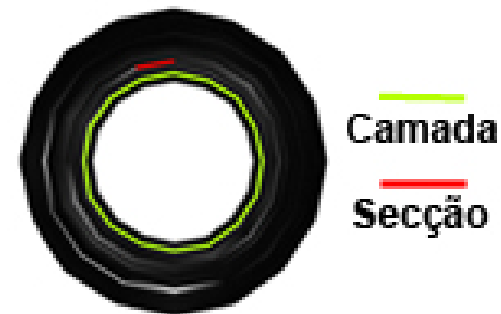
following pre-defined threshold.



## Signal analysis Step 2/3

Calculation of the values that define the different sections of the various layers:

The average amplitude at intervals of 0.25 ms multiplied by 200 indicates the color intensity scale Gray.

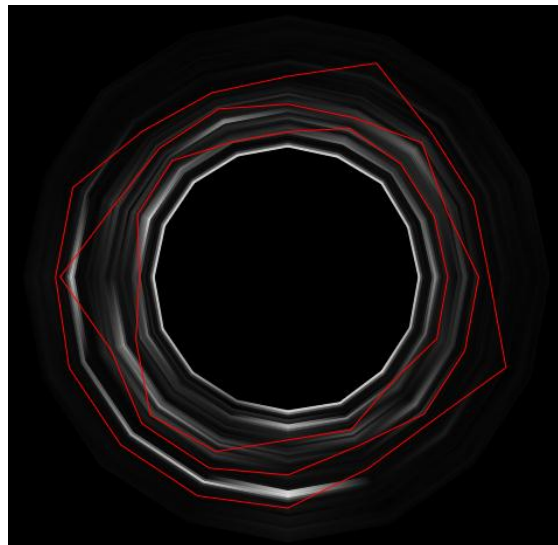


Calculation of the different layers of the intestine:

Using the same formula

$$d = t * 0.75$$

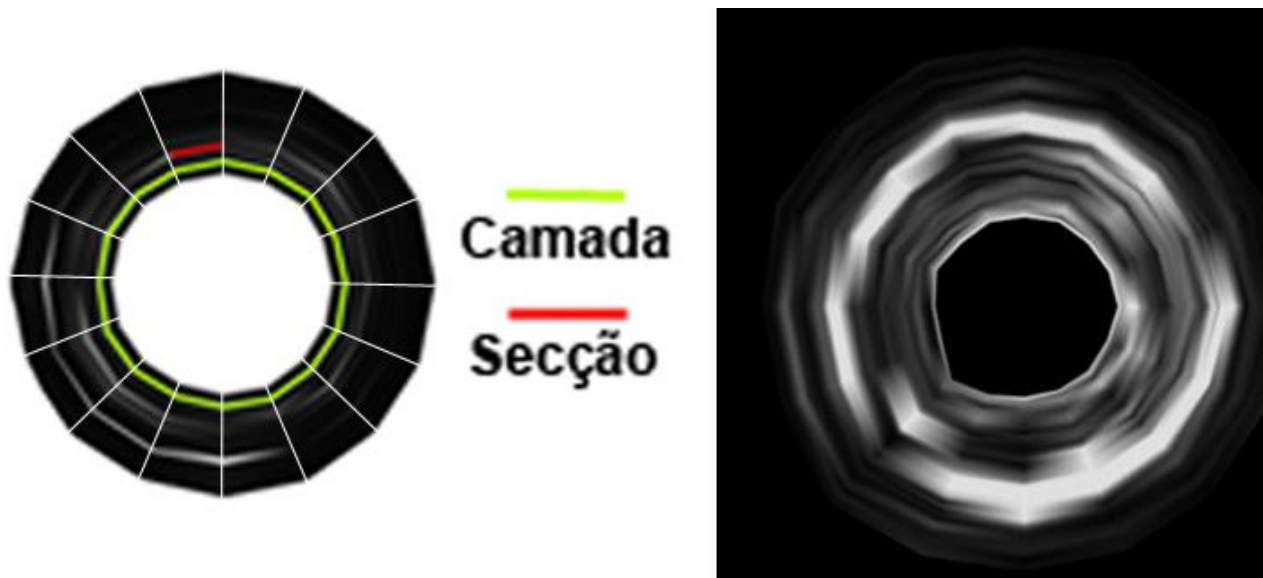
where t is the value of three peaks following the initial contour.





## Final 2D reconstruction

The visual reconstruction of the 2D image is done after the analysis of all fragments.  
The reconstruction is done within a framework OpenGL.



# 3D Reconstruction

Contour detection based on 2D images based on simulated annealing algorithm

Contour detection based on US raw data using information from several consecutive slices

3D rendering based on triangulation of obtained points

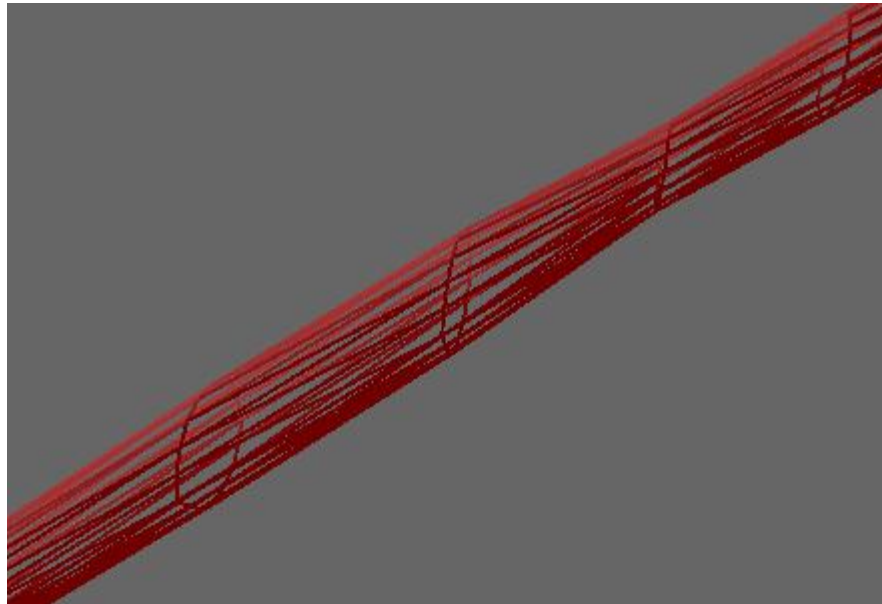
XML writer/parser for writing and reading 3D models

The screenshot shows a Windows-style dialog box titled "Troy Input". It is divided into two main sections. The first section, "Information of patient", contains several input fields: "Reference of capsule:", "Reference of Patient:", "Name:", "Contact:", and "Notes:". There are also radio buttons for "Sex:" (Female and Male) and a dropdown menu for "Age:". The second section, "Create i3DModel", contains two buttons: "Find metadata.." and "Find calibration..", followed by a "Save filename:" text box. At the bottom of the dialog are three buttons: "Start", "Cancel", and "Done".

## 3D Reconstruction

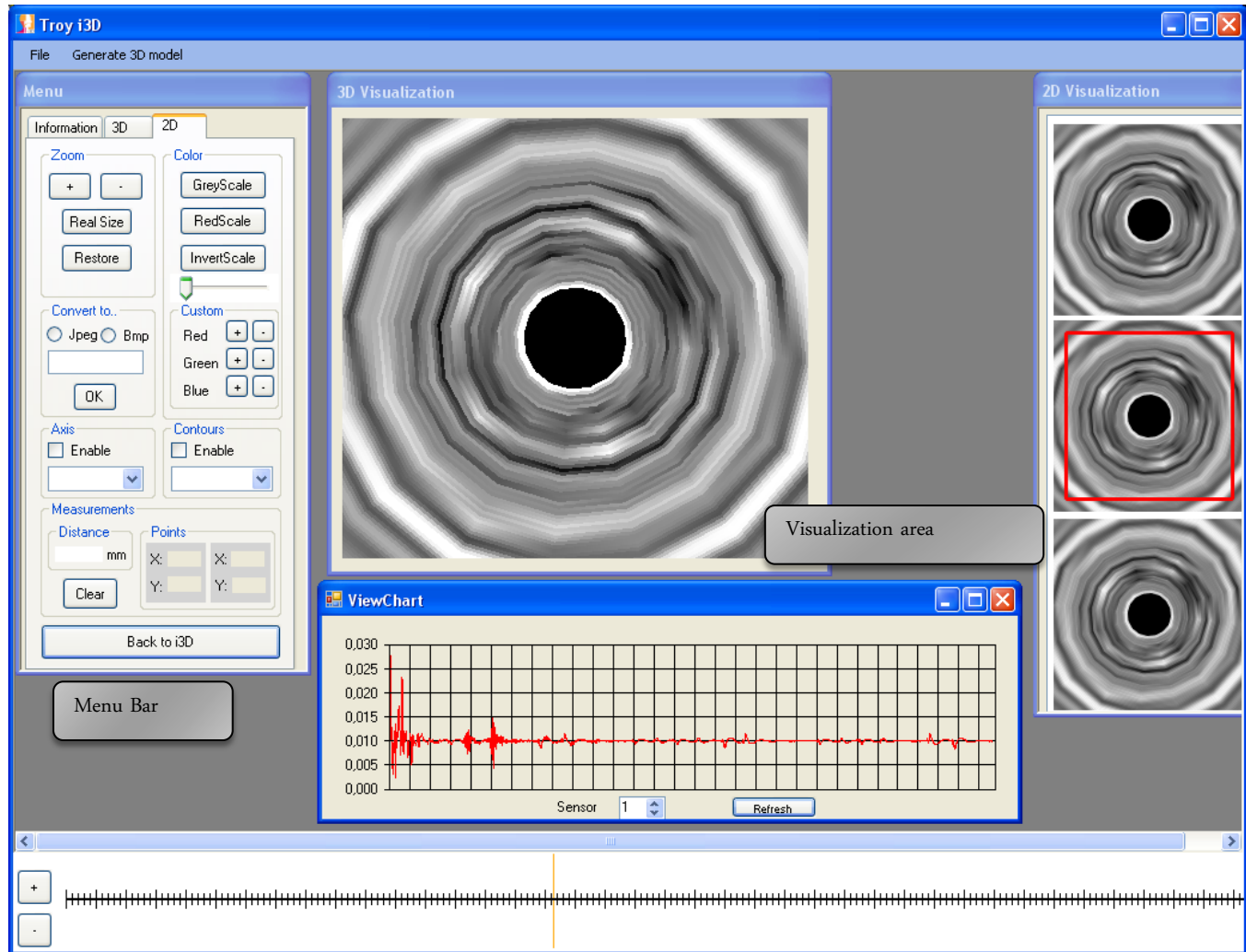
3D reconstruction is based on the triangulation of the contour points positioned in sequential images in accordance with the sensors placed on the abdomen.

The position, orientation and rotation information of each fragment are essential for this reconstruction.



# Presentation layer

- 2D /3D Manipulation;
- Inside view Animation;
- Measures;
- Color scale;
- Visualization Filters;
- Contours;
- Notes;
- Time bar.
- US chart data

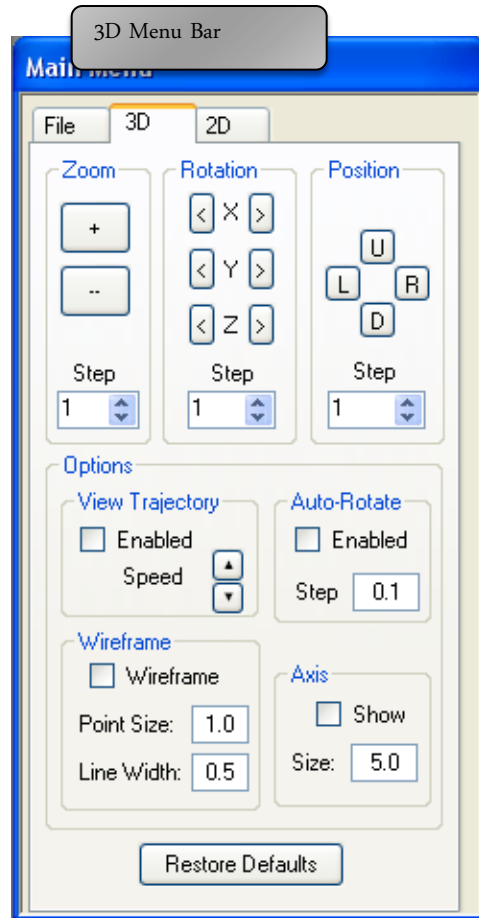


Menu Bar

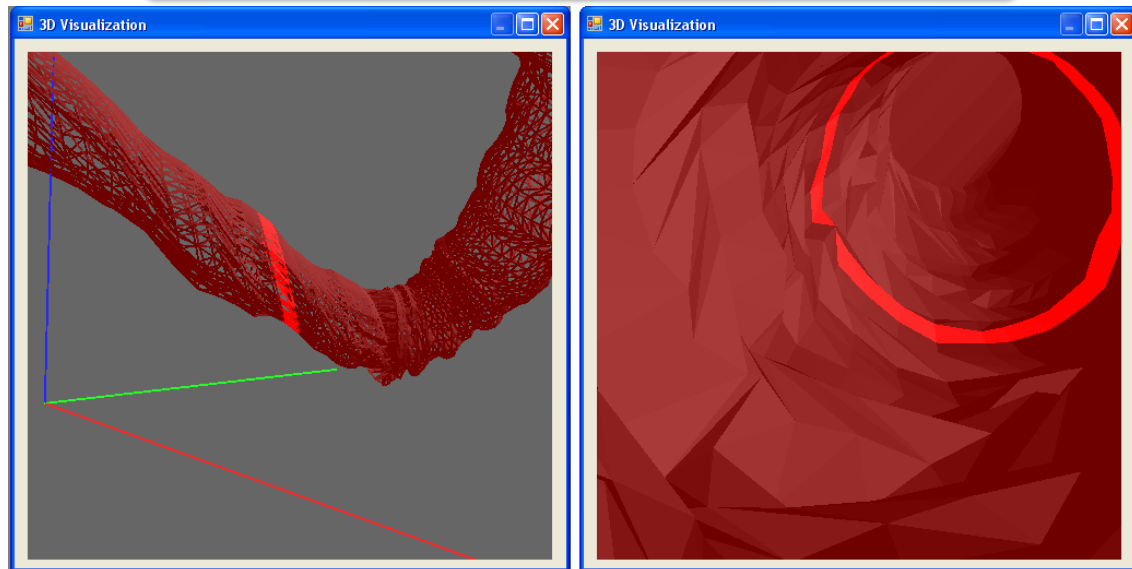
Visualization area

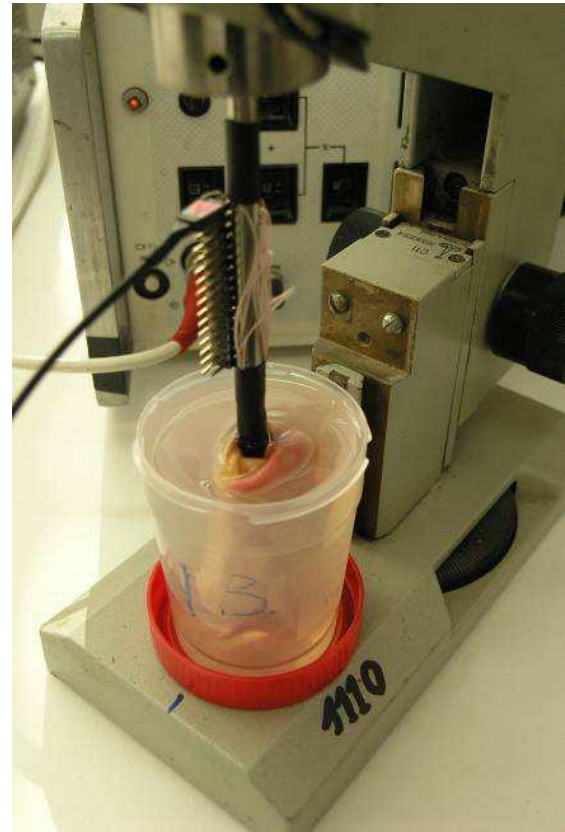
Time Bar

# Presentation layer



3D Visualization area (wireframe and axis; trajectory view)





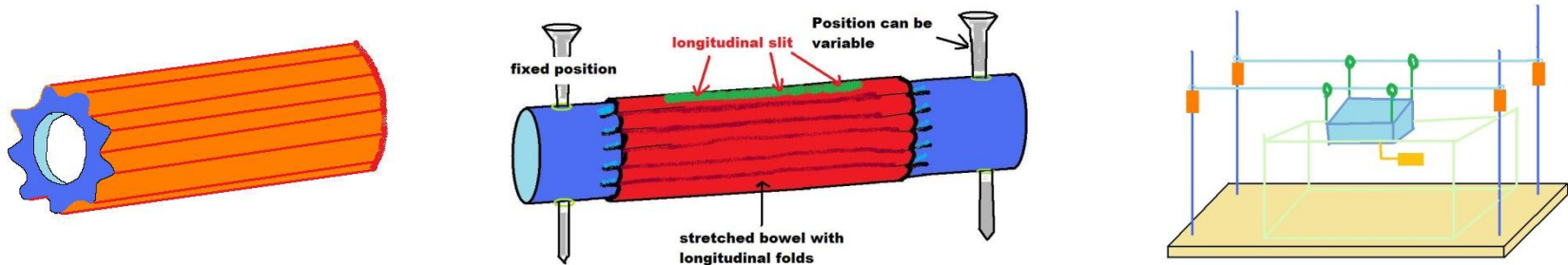
## TESTS

## Planned phantom preparation

16 Longitudinal zones needed for correlation between circumferential sectors of bowel to corresponding crystals/channels.

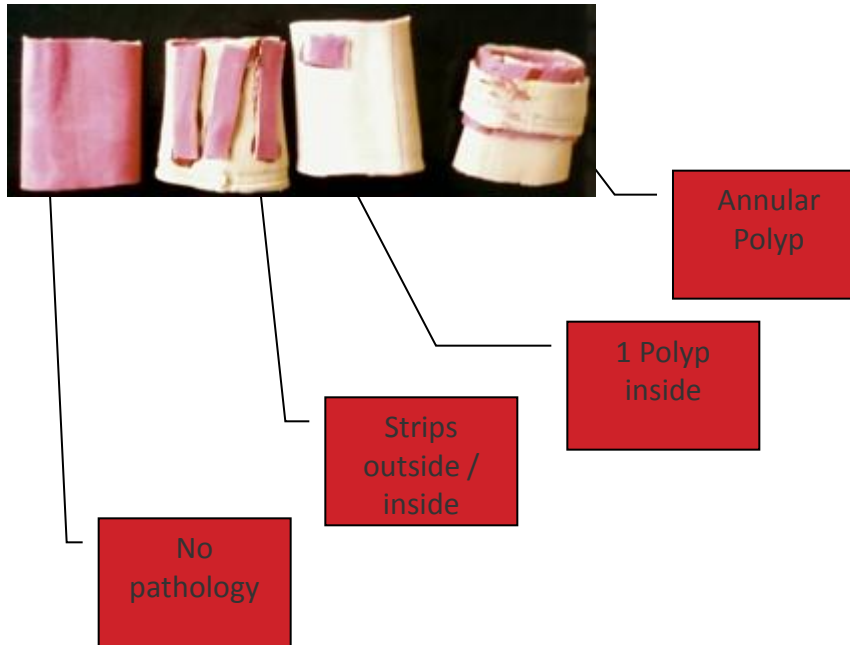
Several (>5) transversal zones corresponding to several positions of capsule during linear manual movement. Their role is to ensure approximate positioning of capsule and to make possible a correlation between position of normal or abnormal segments of bowel to corresponding signals, without seeing the probe.

Longitudinal folds to reshape the bowel.



# Planned Tests

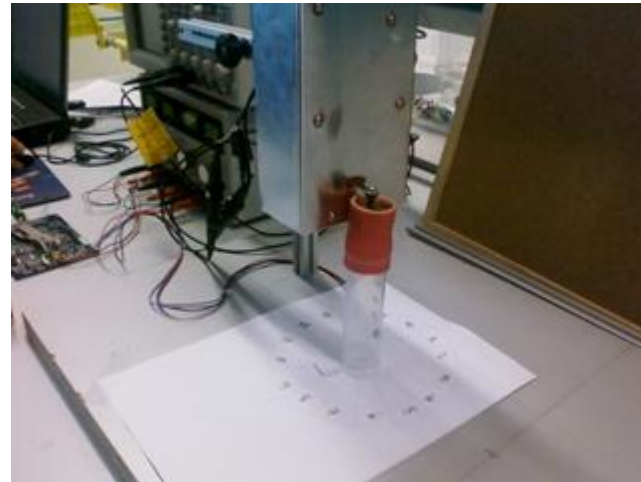
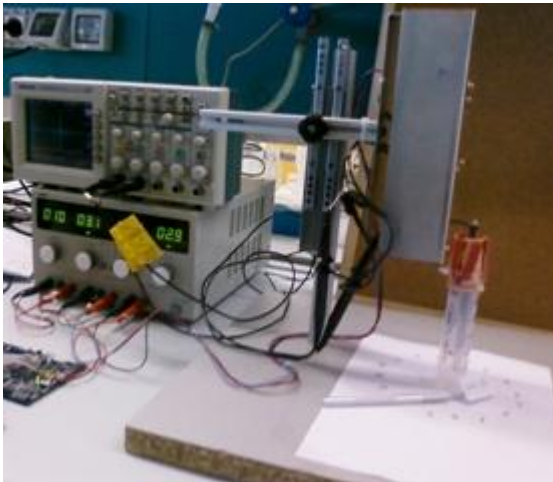
Tests were made to 4 smaller phantoms





## Actual Tests

Setup of the testbed:



### Data acquisition

11 samples collected from each 5 phantoms

With polyp in different positions

With strips inside

With strips outside

With tumour / inflammation (annular polyp)

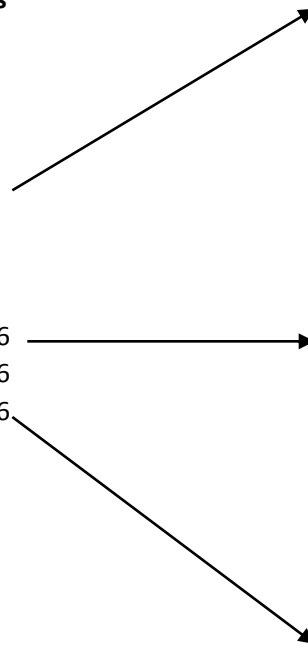
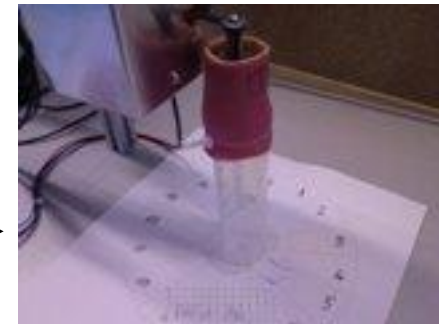
Clean bowel (no pathology)

Each data file contains several captures from the same view (1/second)

1 calibration set

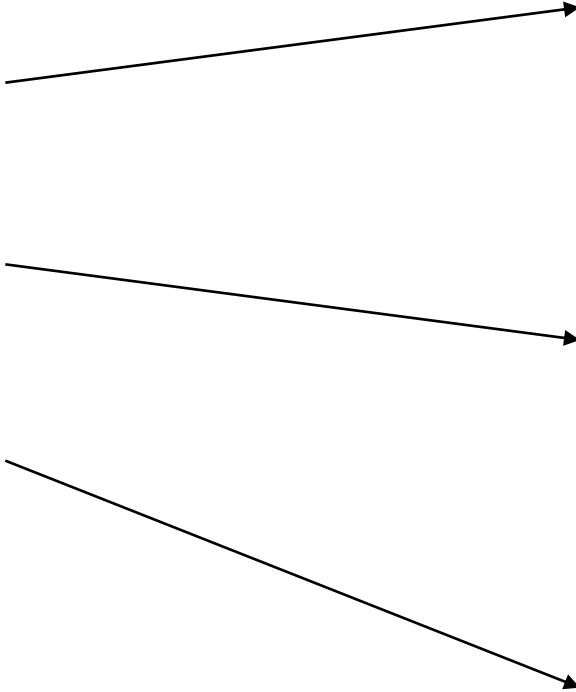
## Data acquisition - Polyp

Data file name	Timing	Description	Other Remarks
Data 28	11:29	no polyp	Polyp in pos 9
Data 29	11:30	no polyp	Polyp in pos 5
Data 30	11:32	no polyp	Polyp in pos 5
Data 31	11:34	no polyp	Polyp in pos 5
Data 32	11:39	no polyp	Polyp in pos 5
Data 33	11:40	no polyp	Polyp in pos 5
Data 34	11:42	no polyp	Polyp in pos 5
Data 35	11:43	no polyp	Polyp in pos 5
Data 36	11:46	with polyp	Polyp in pos 5-6
Data 37	11:48	with polyp	Polyp in pos 5-6
Data 38	11:50	with polyp	Polyp in pos 5-6



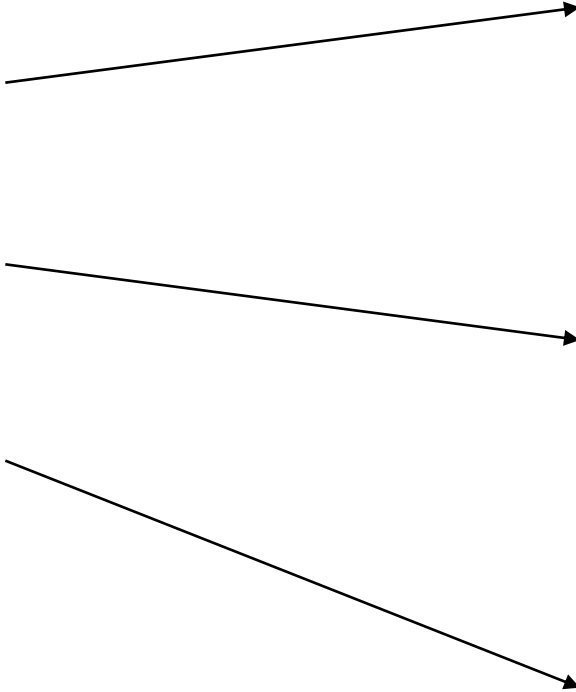
## Data acquisition – Strips inside

Data 39	11:59	with "strips" inside
Data 40	12:00	with "strips" inside
Data 41	12:04	with "strips" inside
Data 42	12:06	with "strips" inside
Data 43	12:09	with "strips" inside
Data 44	12:12	with "strips" inside
Data 45	12:14	with "strips" inside
Data 46	12:16	with "strips" inside
Data 47	12:18	with "strips" inside
Data 48	12:20	with "strips" inside
Data 49	12:22	with "strips" inside



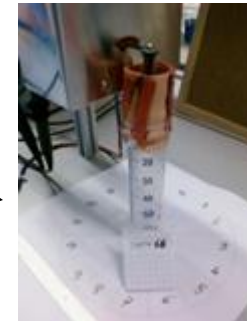
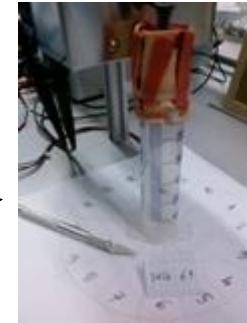
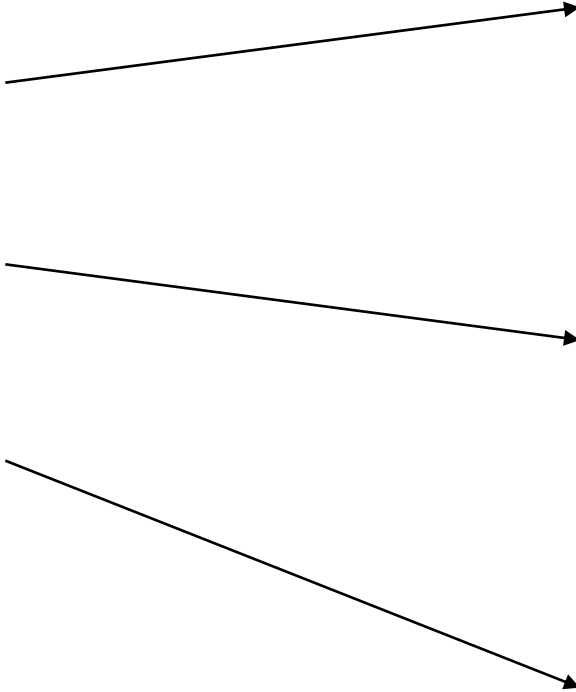
## Data acquisition – Annular Polyp

Data 50	12:28	with tumor/inflammation
Data 51	12:29	with tumor/inflammation
Data 52	12:31	with tumor/inflammation
Data 53	12:32	with tumor/inflammation
Data 54	12:34	with tumor/inflammation
Data 55	12:35	with tumor/inflammation
Data 56	12:36	with tumor/inflammation
Data 57	12:38	with tumor/inflammation
Data 58	12:39	with tumor/inflammation
Data 59	12:41	with tumor/inflammation
Data 60	13:42	with tumor/inflammation



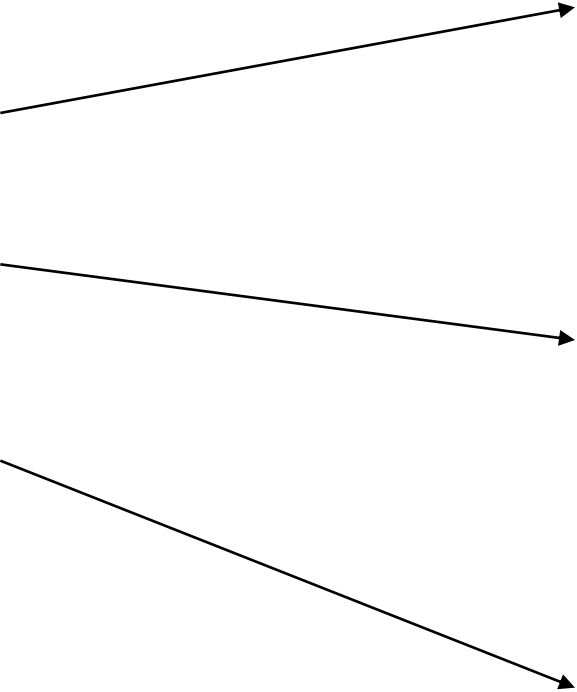
## Data acquisition – Strips outside

Data 61	13:45	with "strips" outside
Data 62	13:46	with "strips" outside
Data 63	13:50	with "strips" outside
Data 64	13:52	with "strips" outside
Data 65	13:57	with "strips" outside
Data 66	13:58	with "strips" outside
Data 67	14:00	with "strips" outside
Data 68	14:07	with "strips" outside
Data 69	14:09	with "strips" outside
Data 70	14:10	with "strips" outside
Data 71	14:12	with "strips" outside
Data 72	14:16	with "strips" outside

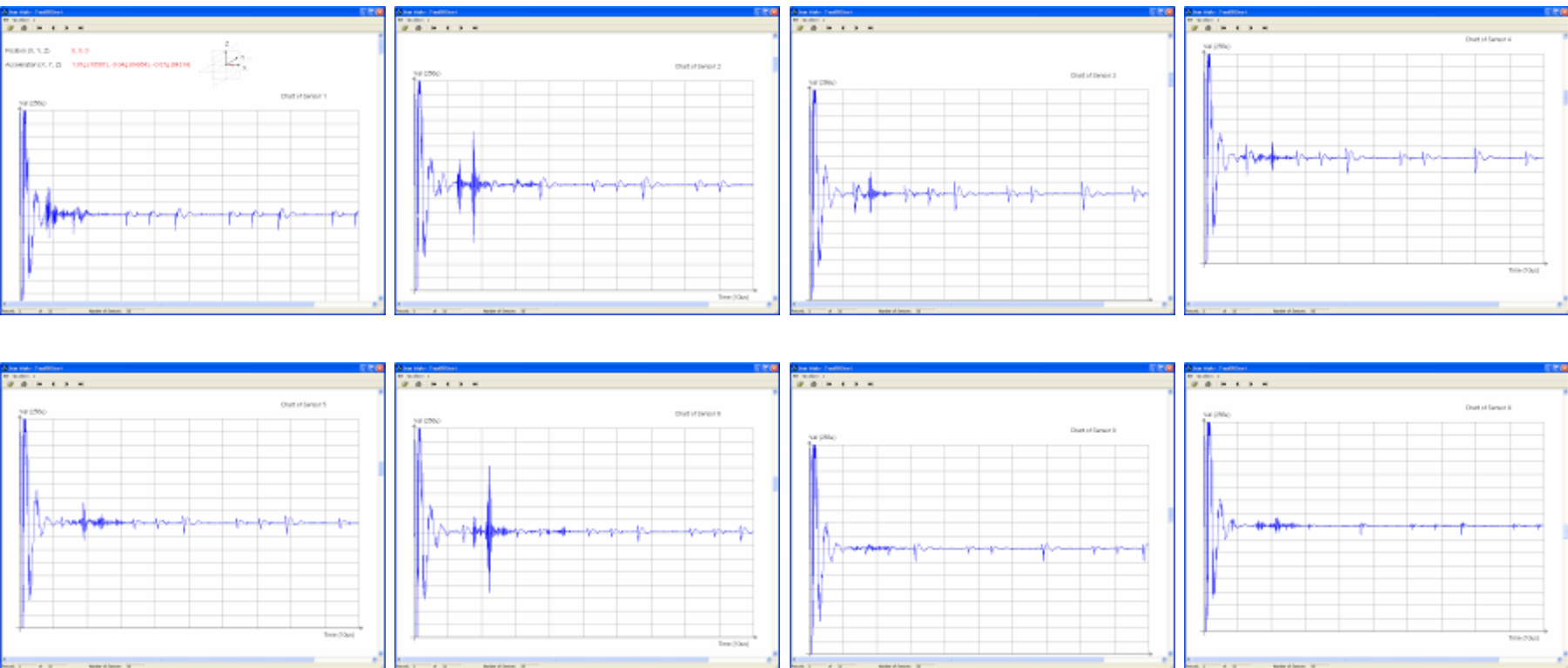


## Data acquisition – No Polyps

A	14:23	Clean bowel
B	14:25	Clean bowel
C	14:26	Clean bowel
D	14:30	Clean bowel
E	14:32	Clean bowel
F	14:33	Clean bowel
G	14:34	Clean bowel
H	14:36	Clean bowel
I	14:37	Clean bowel
J	14:39	Clean bowel
K	14:41	Clean bowel

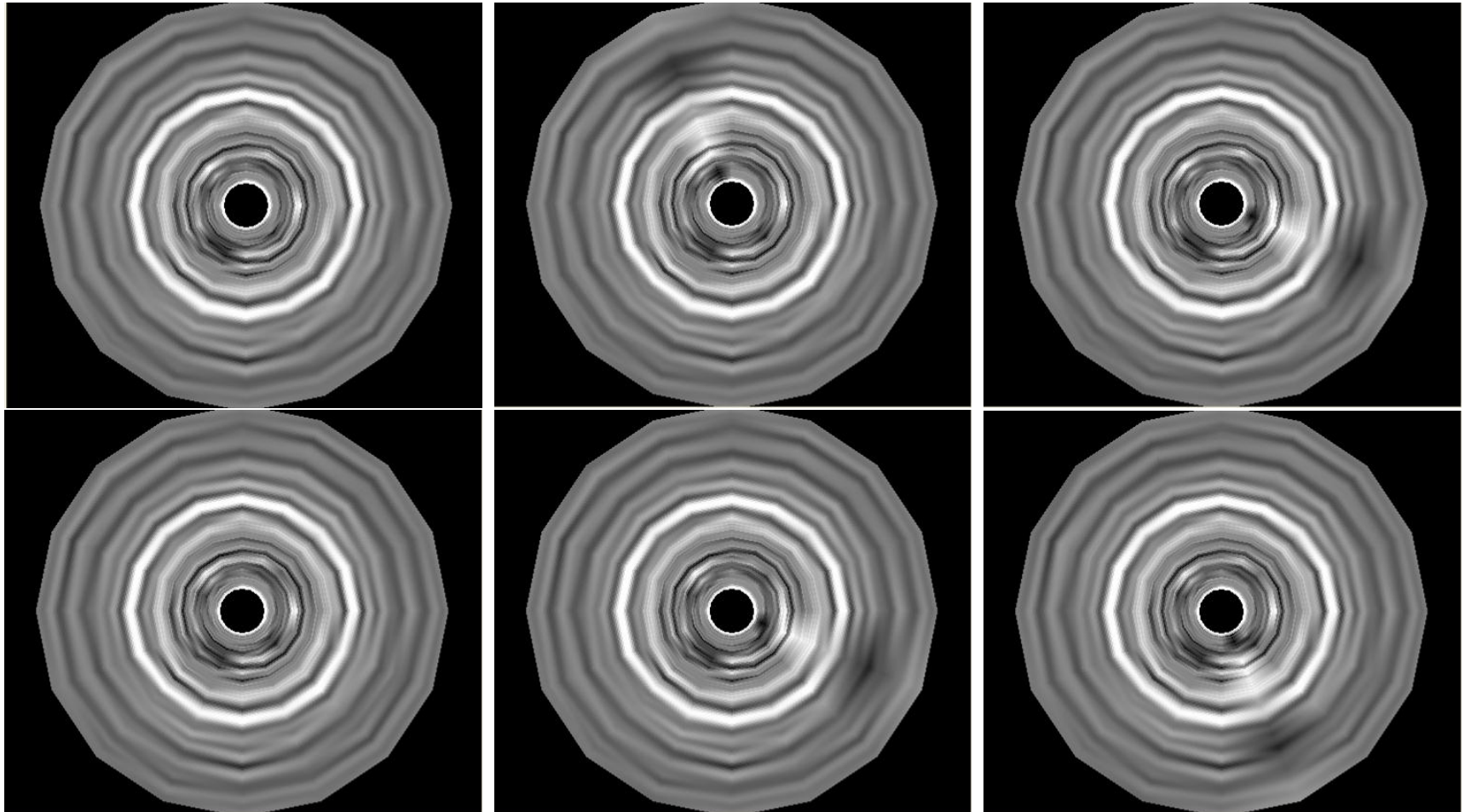


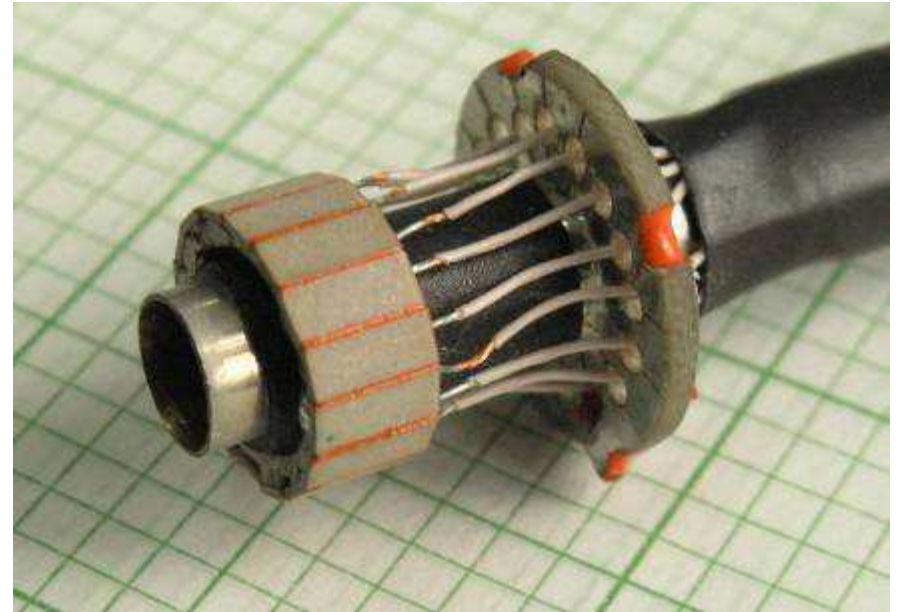
# Tests Results





## Tests Results





## RESULTS AND CONCLUSIONS

## Results / Conclusions

Based on these results it is possible to determine a set of classifiers for the TROY concept and its characterization as a screening test. The most significant parameters, according to Wilson and Jungner, are the following:

- Specificity  $TN/(FP+TN)$ .
- Sensitivity  $TP/(TP+FN)$ .
- Prevalence  $(TP+FN)/(TP+FP+FN+TN)$ .
- Likelihood ratio + sensitivity  $/(1-\text{specificity})$ .
- Likelihood ratio -  $(1-\text{sensitivity})/\text{specificity}$ .
- Positive predictive value  $TP/(TP+FP)$ .
- Negative predictive value  $TN/(FN+TN)$ .
- Pretest odds prevalence  $/(1-\text{prevalence})$ .
- Post-test odds pretest odds x likelihood ratio.
- Post-test probability post-test odds  $/(post\text{-test odds}+1)$ .

1 Wilson J. M. G., Jungner G., "Principles and practice of screening for disease", World Health Organization, Public Health Paper 34 (1968)

2 UCI College of Medicine, "Evidence-based Medicine Guidebook" (2004)

## Results / Conclusions

These parameters were calculated and are presented in the Table:

- The two most important parameters for a screening diagnostic exam are: sensitivity and specificity
- They show that the exam is very accurate in classifying as positive the abnormal cases and as negative the normal cases.
- The other parameters are also very interesting and demonstrate that the TROY system can be a very useful tool for screening possible disorders in the gastrointestinal tract.

Parameter	Value
Specificity	97%
Sensitivity	88%
Prevalence	80%
Likelihood ratio+	31,34
Likelihood ratio -	0,13
Positive predictive value	0,99
Negative predictive value	0,67
Pretest odds	3,91
Post-test odds	122,5
Post-test probability	99%

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